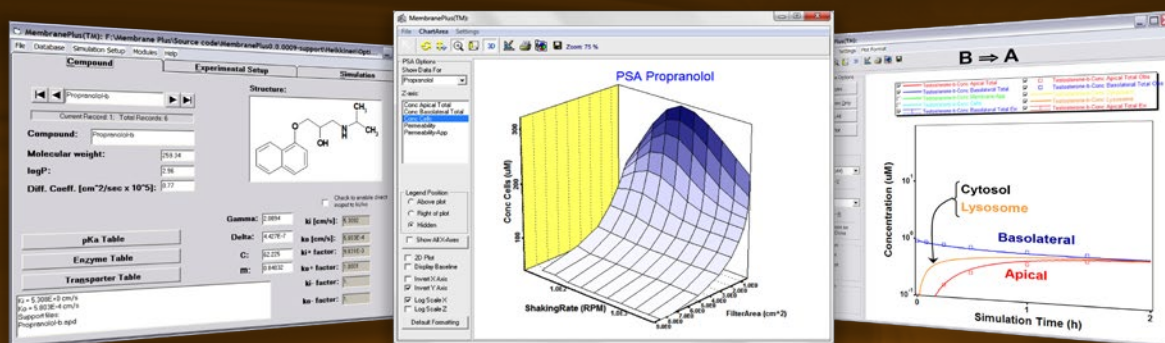


MembranePlus™

in vitro permeability
testing... reimaged!



www.simulations-plus.com



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What is MembranePlus™?

MembranePlus is an advanced, yet easy-to-use, modeling and simulation software program that unlocks important information from your *in vitro* permeability assay studies. With MembranePlus, all relevant experimental and cellular processes, such as protein binding, lysosomal trapping, pH difference, shaking rate, paracellular permeability, and carrier-mediated transport & metabolism, are integrated to simulate drug

concentrations from *in vitro* cell-based/non-cell-based assays and calculate the corresponding permeability & additional *in vivo* rate parameters. The combination of MembranePlus and GastroPlus™ brings you closer to accurately predicting *in vitro* – *in vivo* extrapolation (IVIVE) of absorption processes (both passive and carrier-mediated)!

How can we use it?

Permeability is a critical parameter for absorption, since molecules need to permeate through cellular membranes to reach target sites in the body. For over 20 years, significant research has been devoted to *in vitro* permeability studies, with several guidelines being published and all pharmacopeia describing appropriate methods for testing.

MembranePlus has two primary purposes:

- 1.) Simulation of *in vitro* permeability
 - a. Predict various permeability processes (e.g., paracellular, transcellular)
 - b. Estimate different intracellular concentrations:
 - i. Membrane
 - ii. Cytosol
 - iii. Lysosome
 - c. Assess impact of experimental variability on the predicted outcomes
- 2.) Analysis of measured *in vitro* permeability data
 - a. Identify paracellular and transcellular permeability
 - b. Calculate *in vitro* K_m and V_{max} for enzymes and transporters
 - c. Fit parameters to build a robust model and learn from the data

Who should be using it?

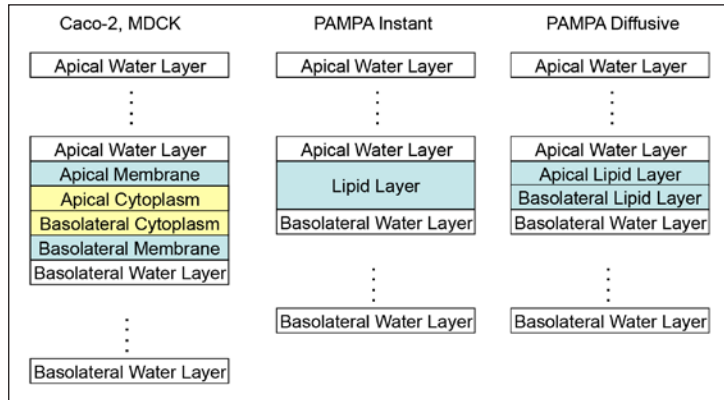
MembranePlus is going to be very helpful for:

- Users of GastroPlus looking to define inputs for more accurate *in vivo* absorption predictions in the Advanced Compartmental Absorption and Transit (ACAT™) model.
- Discovery scientists looking to categorize compounds into high and low permeability classes
- DMPK researchers that focus on *in vitro* transporter/metabolism kinetic studies
- CROs which provide *in vitro* Caco-2, PAMPA, or MDCK permeability services, to assist with the optimization of the experimental design for client studies

Which experiments can we simulate?

MembranePlus has default models describing several common *in vitro* systems:

- 1.) PAMPA (built-in 12, 24, and 96 wells)
- 2.) Caco-2 (built-in 12, 24, and 96 wells)
- 3.) MDCK (built-in 12, 24, and 96 wells)



Of course, use MembranePlus to customize any cell-monolayer based *in vitro* system to mimic your in-house lab!

For the experiment, MembranePlus allows you to control the following during your simulations:

- 1.) pH in donor and receiver compartments
- 2.) Addition of albumin to donor or receiver compartments
- 3.) Shaking/stirring rates
- 4.) Volume of media in donor and receiver compartments
- 5.) Sampling protocols that may impact volume or drug concentrations, including:
 - a. Withdrawal of sample volume
 - b. Replacement of sample volume with blank buffer or original donor solution
 - c. Moving the insert to a different plate with blank buffer in receiving compartment
- 6.) Cell culture time
- 7.) Filter surface area
- 8.) Filter pore size and density

The screenshot displays several overlapping windows from the MembranePlus software:

- Experimental Setup:** A window with tabs for 'Component', 'Experimental Setup', and 'Graph'. It contains various parameters like 'Shaking rate (rpm)', 'Apical volume (µL)', 'Basolateral volume (µL)', 'Cell culture time (days)', 'Apical pH', 'Basolateral pH', 'Filter Area (µm²)', 'Filter Pore Size (µm)', 'Filter Pore Density (Pores/µm²)', 'Filter Membrane Depth (µm)', and 'DRI Layer Thickness (µm)'. A diagram of a well insert is shown with labels for 'Apical Fluid Compartment', 'Transwell Insert', 'Tissue Culture Well Plate', and 'Basolateral Fluid Compartment'.
- Sampling Protocol:** A window titled 'Sampling Protocol' with a 'Sampling Table' and 'Protein Binding Setup' options. A blue box highlights the 'Sampling Table' with text: '-Apical and Basolateral sites can be sampled at the same time', '-Donor side can be replaced by buffer or donor solution', and '-Receiver side can be replaced completely'.
- Protein Binding Model:** A window titled 'Protein Binding Model for Propagator' showing 'Serum Albumin Concentrations [µM]' for 'Apical' and 'Basolateral' compartments. It includes a graph of 'Free Drug Fraction' vs 'Total Conc [µM]' and options for 'Linear binding' and 'Saturable binding'.
- Losses Setup:** A window titled 'Losses Setup' with a list of 'Different types of drug loss can be defined in the simulation':
 - Evaporation from the apical chamber
 - Plastic Binding to the well surface
 - Fast saturable binding: driven by concentration gradients and diffusion
 - Slow saturable binding: driven by concentration
 - Slow infinite binding: driven by concentration
 - Non-Specific Loss: accounts for any other loss of compound.

What drug information is needed for the simulation?

Basic physicochemical properties [e.g., logP/logD, pKa(s), and molecular weight] can be defined through *in vitro* measurements or predicted from chemical structure (through ADMET Predictor™). If including enzymes or transporters in your assay, information about Vmax and Km needs to be entered (or can be “fitted” with measured concentration-time data from your permeability studies)

The screenshot shows the MembranePlus software interface with the following sections:

- Compound:** Selected Compound: Propranolol. Molecular weight [g/mol]: 259.34. Reference logD: 2.96 @ pH: 7. Diff. Coeff. [cm²/sec x 10⁻⁵]: 0.77.
- Experimental Setup:** Includes fields for Enzyme Table and Transporter Table.
- Simulation:** Initial Concentrations: Donor Conc [μM]: 1, Total [μM]: 0.12627; Receiver Conc [μM]: 0, Total [μM]: 0. Passive Transport Model: Gamma [cm/s]: 1.1066, Vi [cm/s]: 7.59E-3, Vo [cm/s]: 3.074E-4, Delta: 3.025E-6, Vmax factor: 1, Km factor: 1, C: 27.326, α: 0.84.

Annotations on the left side of the screenshot:

- In vitro* inputs or calculated from chemical structure (through ADMET Predictor™) - points to the Compound section.
- Vmax and Km for enzyme and transporters (not available for PAMPA assays) - points to the Enzyme and Transporter Tables.
- Advanced Membrane Retention model depends on the entry and exit rate constants – can be estimated from our internal logD-based model or fitted from experimental data - points to the Passive Transport Model section.

The diagram on the right illustrates the Advanced Membrane Retention model across three layers: Basic D5a, Apical layer, and Acidic D5a. It shows the equilibrium between HA⁺, H-A-OH, and AOH⁻ species in the Apical layer and Apical cytosol, with rate constants for transport and conversion.

Lysosomal Trapping - An important consideration

In MembranePlus, lysosomal trapping, a process which can impact a compound's distribution in tissues, can be studied in the simulations.

The diagram shows a cell with a lysosome. The cell cytosol has a pH of 7.4, and the lysosome is neutral with a pH of 4. The lysosome membrane is highlighted, with a note: "30% of the cell volume, same thickness as of cell membrane, roughly 100 per cell". A note also states: "Rate constants correspond to the water-membrane input and output rate".

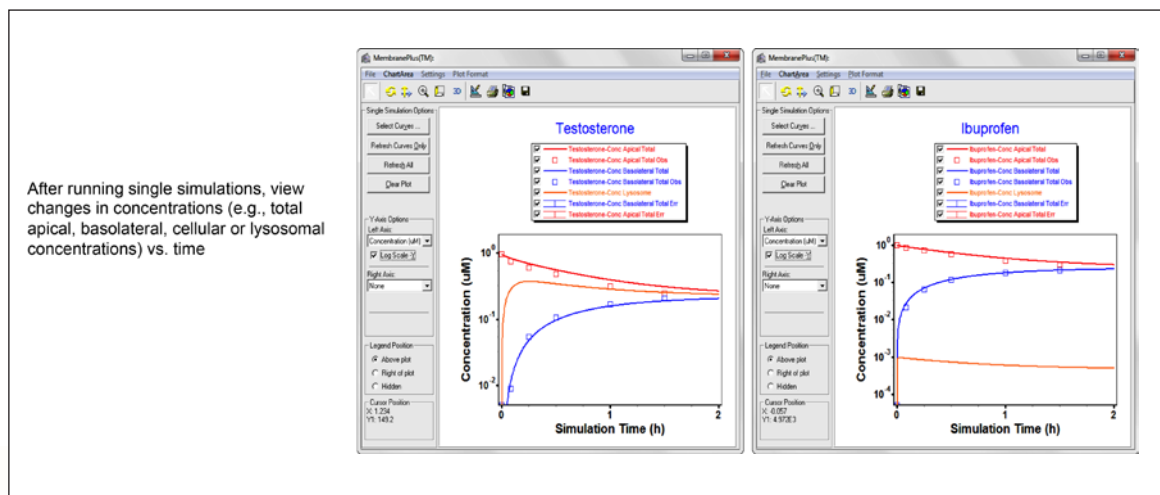
The screenshot of the Lysosome Trapping Model dialog box shows the following settings:

- Cell Membrane Thickness (nm): 30
- Cell Layer Thickness (nm): 16.75
- Cytosol pH: 7.4
- Num Of Lysosomes Per Cell: 100
- Lysosomal Membrane Thickness (nm): 10
- Lysosomal Volume Percentage Per Cell: 30
- Lysosomal pH: 4
- Cell Organelle Percentages: Cell Membrane: 33.07%, Cytosol: 33.44%, Lysosome Membrane: 0.59%, Lysosomal Liquid Phase: 29.45%

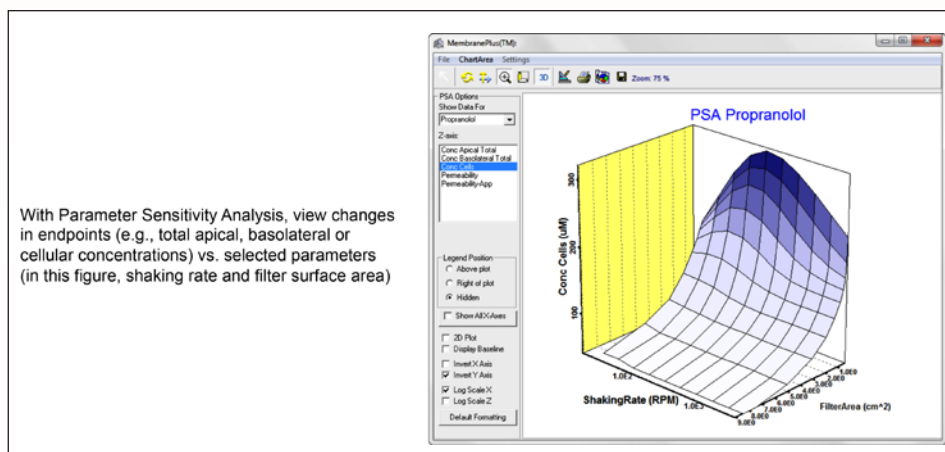
The Simulation Outputs - how does it look?

With MembranePlus, you can run the program in one of several modes:

- **Single simulation:** based on your drug properties (whether measured or predicted through ADMET Predictor™) and experimental setup, easily run a simulation to predict the time course changes in concentrations (e.g., apical, basolateral, cellular, or lysosomal). Also calculate the different permeabilities (transcellular and paracellular).



- **Parameter Sensitivity Analysis:** during early drug development, researchers have a large number of compounds to evaluate and limited resources. With Parameter Sensitivity Analysis, quickly assess the impact of changes to certain properties (e.g., physicochemical or experimental) on critical endpoints. This can help guide your resource allocation plans and identify which experiments should be done next.



- **Batch Simulations:** quickly screen a library of compounds based on predicted permeability or run the same compound through a series of different experiments.
- **Optimization:** an important feature of MembranePlus which turns the program into a fitting routine. Using your measured concentration vs. time data, fit parameters to build more robust models and “learn” from your chemical series.

Regardless of the mode in which you run MembranePlus, report-quality results can be easily generated and shared with others.

T2002

MembranePlus™: A Tool to Study In Vitro/In Vivo Transport and Drug-drug Interaction

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PURPOSE

To develop a mechanistic mathematical model for analysis of *in vitro* permeability assays that accounts for all mechanisms contributing to observed apparent permeability: passive paracellular and transcellular diffusion, carrier-mediated transport, as well as drug accumulation in membranes and some intracellular compartments (e.g., lysosomes). The model was validated by analyzing the effect of competitive inhibition of P-gp by vinblastine on the apparent permeability of indinavir in Caco-2 monolayers.

METHODS

MembranePlus™ (Simulations Plus, Inc.) was used to analyze the concentration-time profiles in donor and receiver compartments after apical and basolateral administration of 50 µg/mL (81.5 µM) indinavir alone and co-administration of 50 µg/mL (81.5 µM) indinavir with 70 µM vinblastine [1]. The physicochemical properties of indinavir and vinblastine were predicted by ADMET Predictor™ 6.0 (Simulations Plus, Inc.). The contribution of paracellular diffusion was estimated from drug properties and the experimental setup. Carrier-mediated transport was modeled with Michaelis-Menten kinetics. The indinavir P-gp Vmax/Km ratio, along with parameters accounting for passive transcellular diffusion and membrane accumulation were fitted to the indinavir-alone data. This basic model was then applied to simulate the inhibition of P-gp by vinblastine by fitting the Vmax/Km ratio for indinavir with competitive inhibition of P-gp by vinblastine. The model also includes various effects of major experiment-related parameters (e.g. shaking rate, solvent pH, filter support and sampling effects).

1. Compound Property



Figure 2. MembranePlus compound tab. The program allows two ways of accounting for passive diffusion through cell membranes: (1) S+ model as listed in Eqn. 1 and 2; and (2) direct transport parameter entries for all neutral and charged species.

The membrane entrance and exit rates are given by Eqn. 1 and 2, as modified from [2] and [3]

$$k_i = \frac{P_{\text{pass}}}{\partial x_{\text{mem}} + 1} + k_o = \frac{\gamma}{\partial x_{\text{mem}} + 1} \quad \text{Eqn. 1}$$

$$P_{\text{pass}} = c(P_{\text{par}})^{\text{fit}} \quad \text{Eqn. 2}$$

2. Transporter Setup

A P-gp efflux transporter is set up in the program transporter table.



3. Experimental Setup

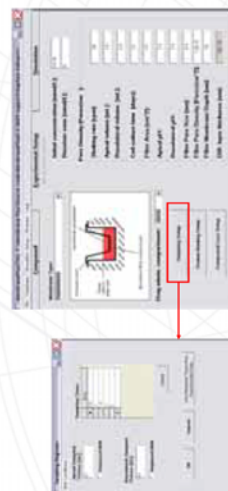


Figure 3. MembranePlus Experimental Setup tab. The program considers major experimental-related parameters, such as shaking rate, apical volume, basolateral volume, filter area, and filter support permeability and etc. As in [1], 0.1 mL samples were drawn from both and basolateral chambers at 0.5, 1, 1.5, 3 and 5 hours.

4. Paracellular and filter permeability

Both paracellular and filter permeabilities are accounted for in the program. The default paracellular model is the Zhimin model [4], which accounts for the molecule mean projected radius and the hydrodynamically equivalent sphere radius. The filter permeability calculation was adopted from [5]. Therefore, the effective paracellular permeability is given by

$$\frac{1}{P_{\text{par}}^{\text{eff}}} = \frac{1}{P_{\text{par}}} + \frac{1}{P_{\text{filter}}} \Rightarrow \frac{1}{P_{\text{par}}^{\text{eff}}} = \frac{P_{\text{par}} + P_{\text{filter}}}{P_{\text{par}} P_{\text{filter}}}$$

where

$$P_{\text{par}}^{\text{eff}} = \frac{\epsilon_p \cdot D \cdot F(r/R_c)}{h_p}$$

$F(x) \rightarrow$ Renkin Function

RESULTS

R² for indinavir-alone data was 99.2% (A->B) and 88% (B->A) and R² for vinblastine inhibition data was 91.1% (A->B) and 85.1% (B->A). The ratio between the two transport fluxes has been calculated to be ~50, indicating a strong P-gp inhibition effect by vinblastine.

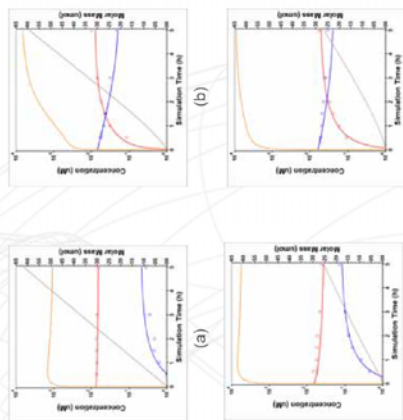


Figure 3. 5-hour simulation of indinavir profiles after (a) apical administration of indinavir, (b) basolateral administration of indinavir, (c) apical administration of indinavir and vinblastine and (d) basolateral administration of indinavir and vinblastine. Red: apical concentration; blue: basolateral concentration; orange: lysosomal concentration; purple: amount transported by P-gp transporter.

CONCLUSIONS

MembranePlus accurately simulated the results of *in vitro* experiments with respect to a variety of mechanisms affecting measured apparent permeability. It is a promising tool in drug research and development. By separating the system-specific from drug-specific parameters in description of drug permeation through the cell membranes it allows obtaining "clean" drug-specific properties (i.e. intracellular Km for efflux transporters) that will allow more direct *in vitro-in vivo* extrapolation and predictions of absorption and drug-drug interactions.



References:
 [1] S. Kaplitz et al., *European Journal of Pharmacology and Biopharmaceutics* 66, 2007, 145-158
 [2] S. Balazs et al., *General Physiology and Biophysics* 6, 1997, 65-77
 [3] H. Zimin et al., *Journal of Pharmaceutical Sciences* 71, 1982, 92-93
 [4] H. Zimin et al., *Journal of Pharmaceutical Sciences* 71, 1982, 42-47
 [5] A. Adson et al., *Journal of Pharmaceutical Sciences* 84 (10), 1995, 1197-1204

MembranePlus™: A tool to Study *in vitro/in vivo* Transport and Lysosomal Trapping

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PURPOSE

To develop a mechanistic mathematical model for analysis of *in vitro* permeability assays that accounts for all mechanisms contributing to observed apparent permeability: passive paracellular and transcellular diffusion, ionization effects, carrier-mediated transport, and metabolism, as well as drug accumulation in membranes and some intracellular compartments (e.g., lysosomes). The model was applied to analyze the effects of lysosomal trapping on the measured apparent permeability of propranolol.

METHODS

MembranePlus™ (Simulations Plus, Inc.) was used to analyze the concentration-time profiles in donor and receiver compartments after apical and basolateral administration of ibuprofen, testosterone and propranolol alone, as well as propranolol in the presence of bafilomycin [1]. The physicochemical properties of propranolol, ibuprofen, and testosterone were predicted by ADMET Predictor™ 6.0 (Simulations Plus, Inc.). The contribution of paracellular diffusion for each drug was estimated from drug properties and the experimental setup. Parameters accounting for passive transcellular diffusion and membrane/lysosomal accumulation were fitted to the propranolol, ibuprofen, and testosterone alone data. This basic model was then applied to explore the effect of bafilomycin on lysosomal pH and the subsequent change in propranolol accumulation in lysosomes. The model includes various effects of the experimental setup (i.e., shaking rate, solvent pH, filter support, sampling effects, etc.) on measured apparent permeability.

1. Compound Properties



The program allows two ways of accounting for passive diffusion through cell membranes: (1) the S+ model as shown in Eqn. 1 and 2; and (2) direct transport parameter entries for all neutral and charged species.

The membrane entrance (K) and exit rates (Ko) are given by Eqn. 1 and 2, as modified from [2] and [3], where P_{par} , P_{mem} are the octanol-water and membrane-water partition coefficients, and c, m, γ and δ are fitting coefficients.

$$k_1 = \frac{P_{par}}{\delta P_{mem} + 1} k_o = \frac{\gamma}{\delta P_{mem} + 1}$$

$$P_{mem} = c(P_{par})^m$$

References:

[1] A.T. Hollomon, *PhET* 328, 2005, 852-892
 [2] S. Balazs et al., *General Physiology and Biophysics* 6, 1997, 65-77
 [3] H. Kuboye et al., *Journal of Pharmaceutical Sciences* 97 (2), 1977, 202-3

2. Experimental Setup



Figure 2. MembranePlus Experimental Setup tab. The program considers major experiment-related parameters, such as shaking rate, apical volume, basolateral volume, filter area, filter support permeability, etc.

3. Diffusion Model

The unstirred layer thicknesses are automatically calculated after the relevant experimental parameters are entered: shaking rate, apical and basolateral volumes, filter area. Therefore, in the current program, the apical and basolateral compartments are separated into a well-stirred layer and a diffusion layer. This diffusion layer is then divided into a number of thinner sublayers to allow accurate calculation of diffusion across the layers according to Fick's Second Law, where c is the concentration and D is the diffusion coefficient.

$$\frac{\partial c}{\partial t} = D \frac{\partial^2 c}{\partial x^2} \quad (\text{Fick's Second Law})$$

4. Paracellular and filter permeability

Both paracellular and filter permeabilities are accounted for in the program. The default paracellular model is the Zhimin model [4], which accounts for the molecule's mean projected radius and the hydrodynamically equivalent sphere radius. The filter permeability calculation was adopted from [5]. The total effective paracellular permeability is given by



$$P_{par}^{eff} = \frac{1}{\frac{1}{P_{par}} + \frac{1}{P_{filter}}} \rightarrow P_{par}^{eff} = \frac{P_{par} P_{filter}}{P_{par} + P_{filter}}$$

where P_{par} and P_{filter} are the paracellular and filter permeabilities, r is the molecular radius, R_F is the filter pore radius, ϵ_F is the filter porosity and h_F is the filter pore depth.

$F(x) \rightarrow$ Renkin function

Results

The membrane transport model (c, m, γ , and δ) was fitted to apical and basolateral administrations of ibuprofen, testosterone and propranolol simultaneously (6 profiles). The fitted concentration-time profiles showed a good match to the experimental data (Figure 3). The overall R^2 for all the concentrations was over 0.9. The same model was then applied to co-administration of propranolol and bafilomycin, suggesting that bafilomycin caused an increase in lysosomal pH from 4 to 5.5 (Figure 4), which resulted in a good match of propranolol concentration-time profiles measured in the presence of bafilomycin.

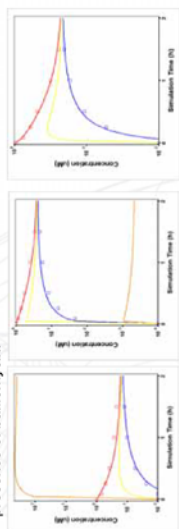


Figure 3. Simulated (lines) and *in vitro* (squares) concentration-time profiles after apical administration of 1 μ M (a) propranolol (b) ibuprofen and (c) testosterone. Simulated apical, basolateral, cytosol and lysosomal concentrations are shown in red, blue, yellow and orange respectively. Note that in (c), cytosol and lysosomal concentrations are overlapping. A similar match between simulated and observed profiles was obtained for basolateral administration (data not shown).

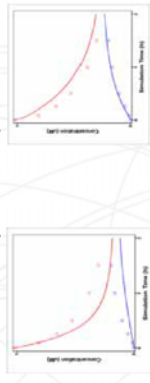


Figure 4. Predicted (lines) and *in vitro* (squares) concentration-time profiles after apical administration of 1 μ M propranolol in the presence of 100 nm bafilomycin. (a) lysosomal pH set to be 4, (b) lysosomal pH set to be 5.5. Simulated apical, basolateral concentrations are shown in red and blue, respectively. A similar match between simulated and observed profiles was obtained for basolateral administration (data not shown).

CONCLUSIONS

MembranePlus has enabled the ability to analyze *in vitro* experiments with respect to the variety of mechanisms affecting measured apparent permeability. The current study shows that it is a promising tool in drug research and development for *in vitro-in vivo* extrapolation, not only in prediction of absorption, but also other processes affecting drug distribution in different tissues (e.g., lysosomal trapping).



