

Physiologically Based Biopharmaceutics Modeling and Virtual Bioequivalence Assessment to Support Formulation Development

Joyce Macwan, Ph.D.

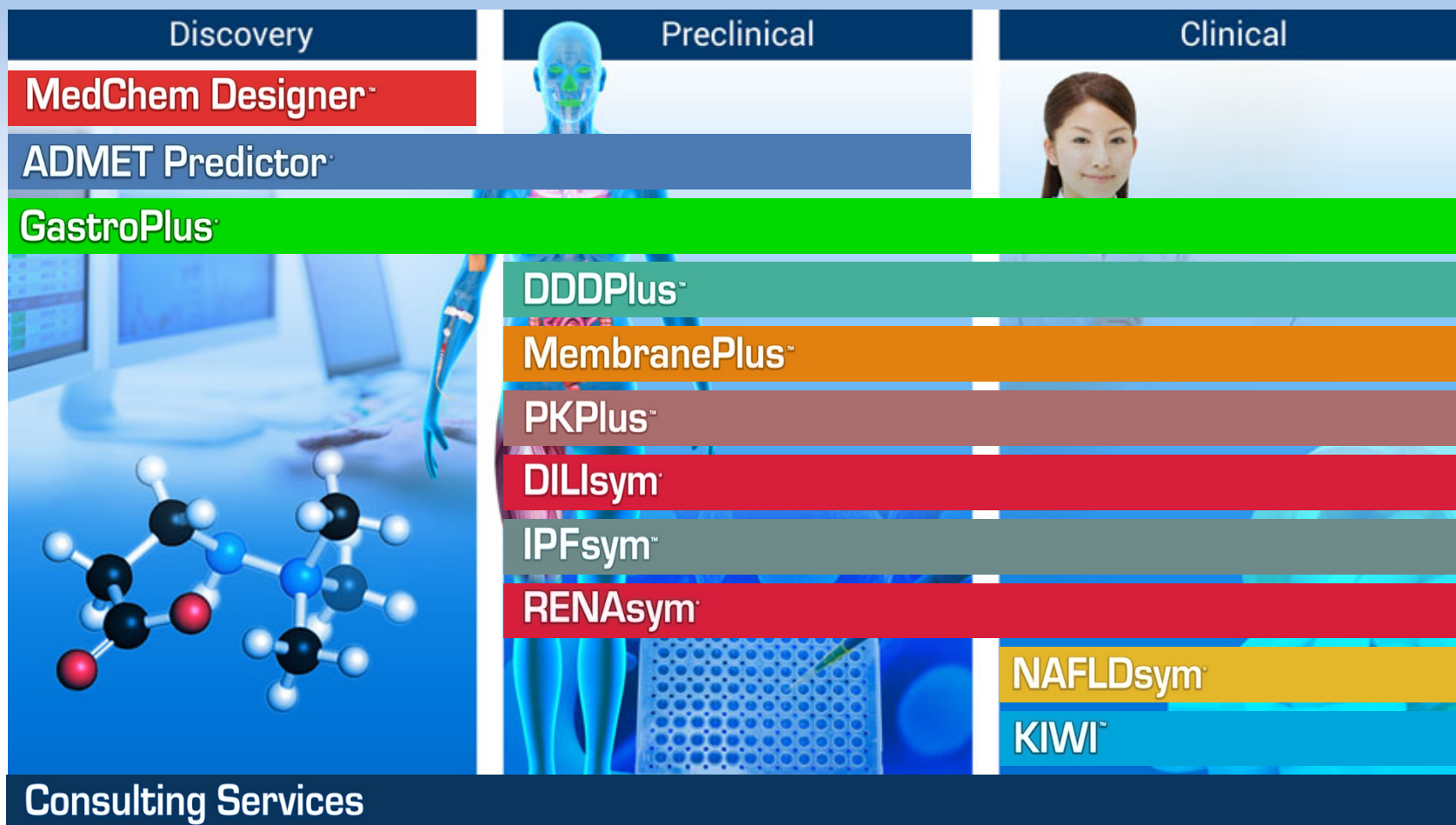
Simulations Plus, Inc.

USA

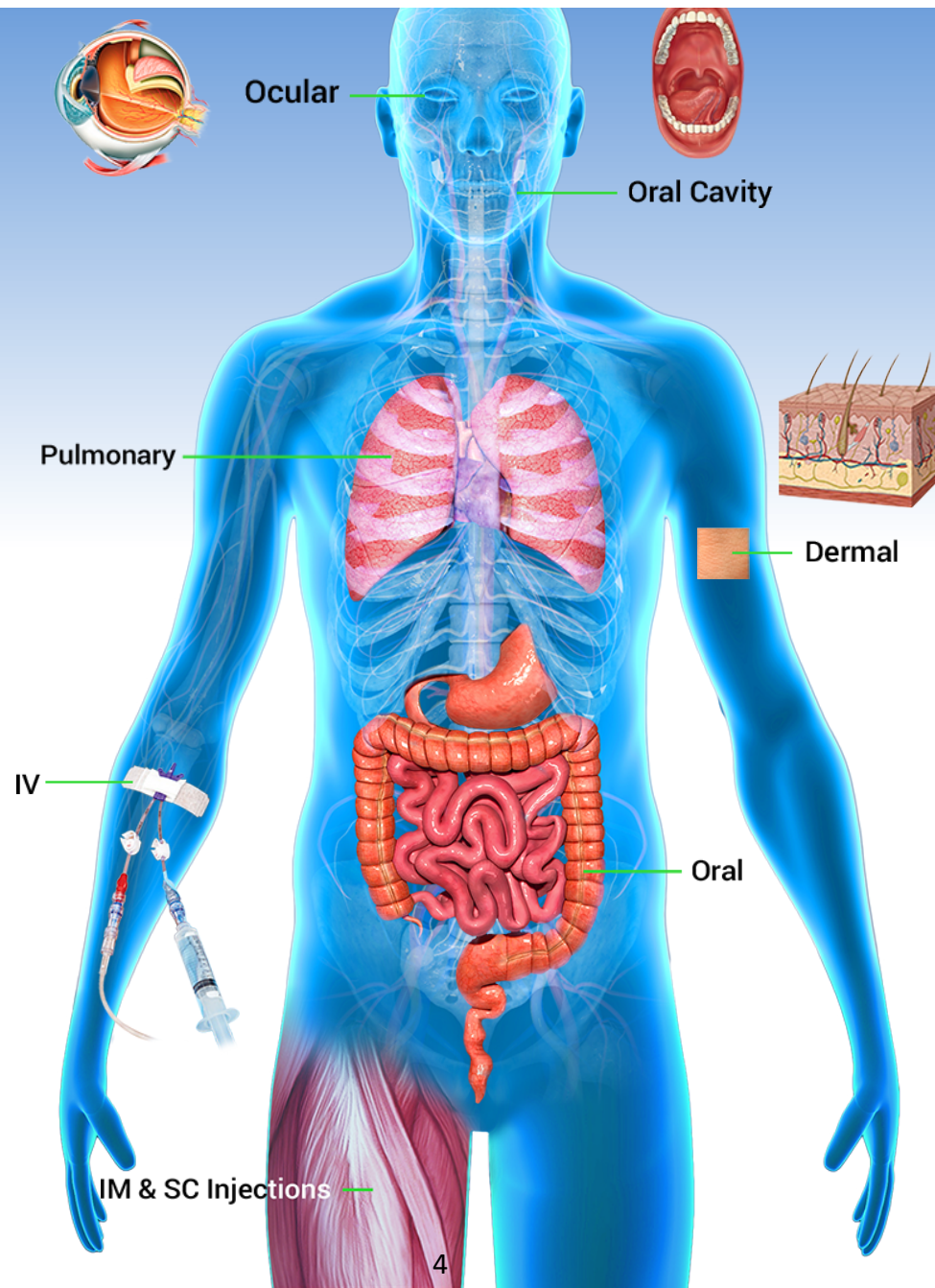
Outline

- **Introduction**
- **Mechanistic Absorption and PK modeling using GastroPlus®**
- **Overview of regulatory submissions**
- **Industrial applications of MAM/PBPK modeling – case studies**
- **Conclusions**

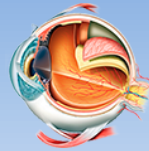
Software and Consulting Solutions from Discovery to Formulation Development



PBBM models defined around the body in GastroPlus®



Funded Collaborations



Ocular



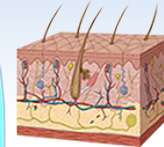
Oral Cavity

FDA: Ocular model extensions

Cosmetics Europe: Dermal model extensions

Pulmonary

Large Pharma: Pulmonary model extensions



Dermal

FDA: Dermal product critical quality attributes

IV

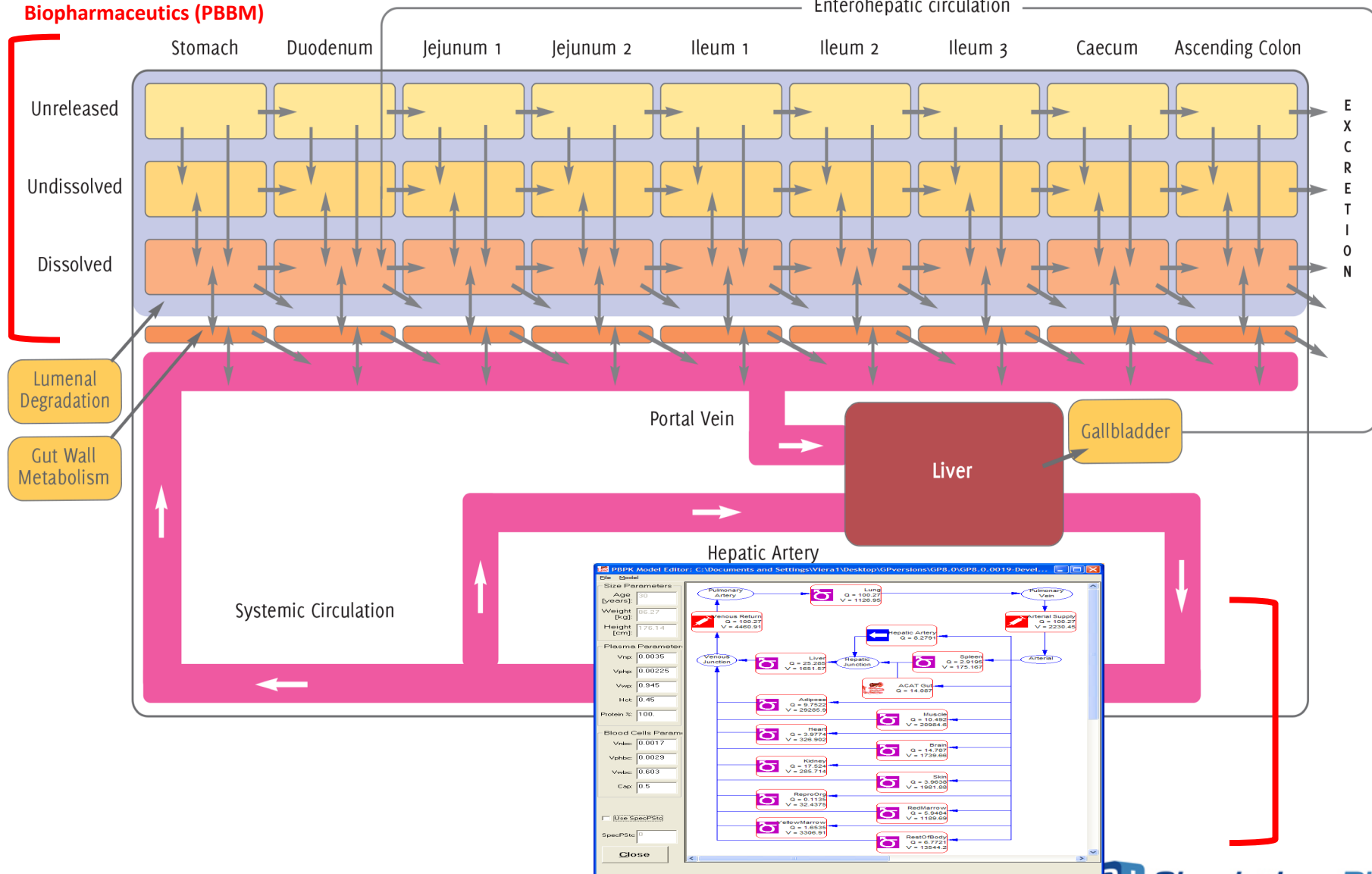
Oral

FDA: LAI model enhancements

IM & SC Injections

Advanced Compartmental Absorption and Transit Model (ACAT™)

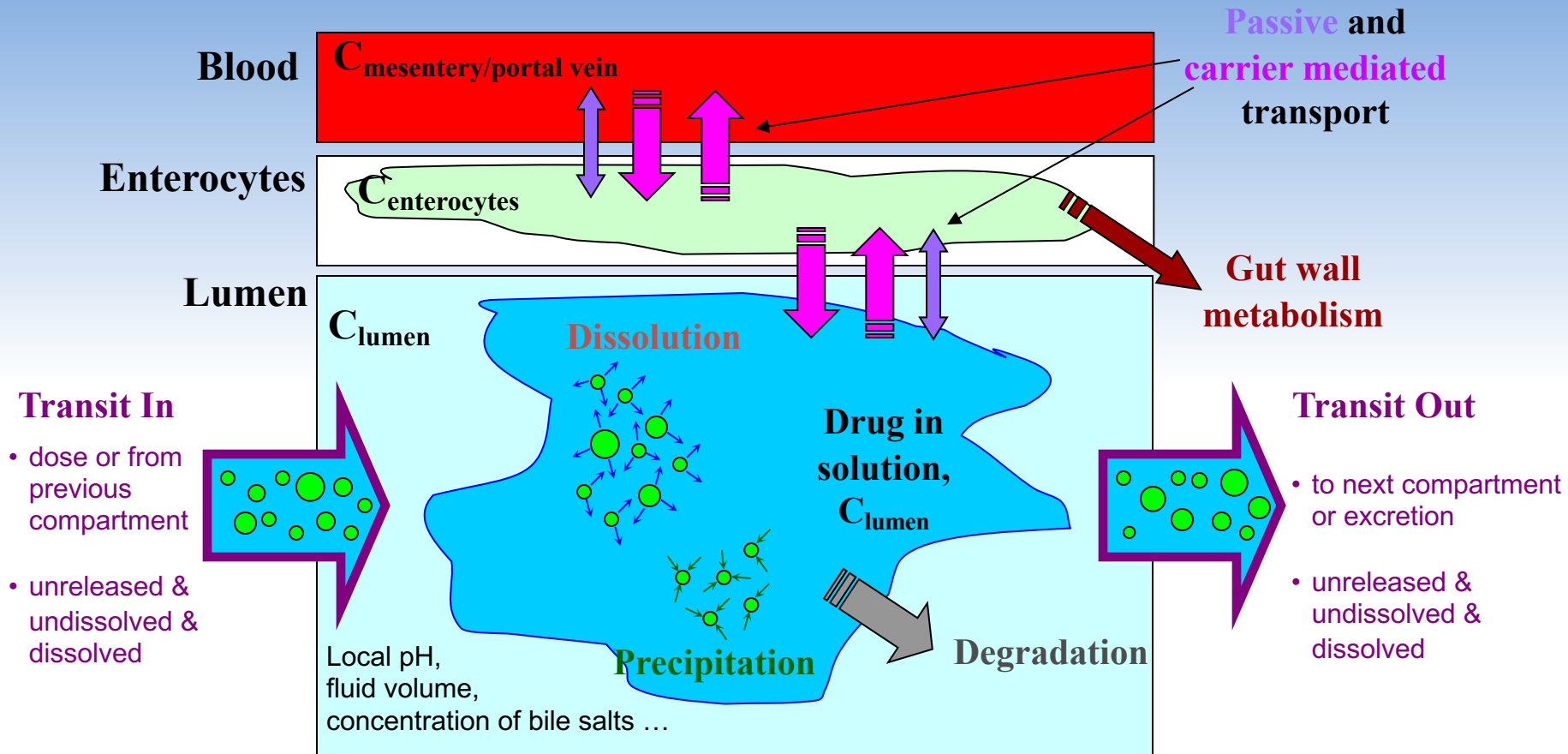
**Physiologically Based
Biopharmaceutics (PBBM)**



**Physiologically based
Pharmacokinetics (PBPK)**

SimulationsPlus
SCIENCE + SOFTWARE = SUCCESS

Processes Involved in Oral Absorption



These phenomena:

- are happening simultaneously
- are repeated in each of the compartments of the gastrointestinal tract

Fed State – ACAT™ Model Changes

GastroPlus(TM): AZD0865-VL.mdb (C:\Doc...\Viera1\Des...\GPv...\GP8.0\GP8...\...)

File Edit Database Simulation Setup Controlled Release Tools Modules (Optional) Help

Compound Gut Physiology-Hum Pharmacokinetics Simulation Graph

Compartmental Parameters

Hum PO 1 mpk soln. Reset All Values Excrete all un-absorbed drug at the end of gut transit time
 Zero-order gastric emptying

| Compartment Data | | | | | | | | | | | | | Enzyme and Transporter Regional Distributions | |
|------------------|------|-------|------|------------------|-------------|-------------|-------------|-------|----------------|------------|-----------------------------|------------|---|----------|
| Compartment | Peff | ASF | pH | Transit Time (h) | Volume (mL) | Length (cm) | Radius (cm) | SEF | Bile Salt (mM) | Pore R (Å) | Poros/L (cm ⁻¹) | Comp. Type | 3A4 Expr | 3A4 Turn |
| Stomach | 0 | 0.0 | 4.90 | 1.00 | 1000.0 | 3.00 | 10.00 | 1.000 | 0.0 | 2.200 | 2.580 | Stomach | 0.0 | 5.0E-4 |
| Duodenum | 0 | 2.630 | 5.40 | 0.26 | 48.25 | 15.00 | 1.60 | 4.235 | 14.44 | 10.41 | 48.64 | Intestinal | 2.09E-3 | 5.0E-4 |
| Jejunum 1 | 0 | 2.616 | 5.40 | 0.95 | 175.3 | 62.00 | 1.50 | 3.949 | 12.02 | 9.640 | 38.90 | Intestinal | 3.26E-3 | 5.0E-4 |
| Jejunum 2 | 0 | 2.615 | 6.00 | 0.76 | 139.9 | 62.00 | 1.34 | 3.489 | 10.46 | 8.400 | 26.09 | Intestinal | 3.26E-3 | 5.0E-4 |
| Ileum 1 | 0 | 2.594 | 6.60 | 0.59 | 108.5 | 62.00 | 1.18 | 3.029 | 7.280 | 7.160 | 16.46 | Intestinal | 1.03E-3 | 5.0E-4 |
| Ileum 2 | 0 | 2.574 | 6.90 | 0.43 | 79.48 | 62.00 | 1.01 | 2.569 | 5.990 | 5.920 | 9.540 | Intestinal | 1.03E-3 | 5.0E-4 |
| Ileum 3 | 0 | 2.513 | 7.40 | 0.31 | 56.29 | 62.00 | 0.85 | 2.109 | 0.730 | 4.680 | 4.896 | Intestinal | 1.03E-3 | 5.0E-4 |
| Caecum | 0 | 1.416 | 6.40 | 4.50 | 52.92 | 13.75 | 3.50 | 1.790 | 0.0 | 3.920 | 2.915 | Colon | 3.1E-4 | 5.0E-4 |
| Asc Colon | 0 | 3.044 | 6.80 | 13.50 | 56.98 | 29.02 | 2.50 | 2.480 | 0.0 | 3.500 | 3.220 | Colon | 3.1E-4 | 5.0E-4 |

C1-C4: 0.06944 0.43028 0.12147 0.46632

Physiology: Human - Physiological - Fed

ASF Model: Opt logD Model SA/V 6.1

Qh (L/min): 1.4

Percent Fluid in SI: 40 Colon: 10

Main changes between Fasted and Fed state (default = moderate-fat meal):

- Higher stomach volume
- Changes in pH (stomach and upper SI)
- Longer gastric emptying
- Higher bile salt concentrations
- Increased liver blood flows

Built-in Fed Physiologies for Different Meal Types

GastroPlus(TM): GastDemo0.mdb (C:\Users\jullin\Docum...\CodeR...\Gastr..)

File Edit Database Simulation Setup Controlled Release Tools Modules (Optional) Help

Compound Gut Physiology-Hum Pharmacokinetics Simulation Graph

Compartmental Parameters

Propranolol HCl

Reset All Values Excrete all unabsorbed drug at the end of gut transit time Zero-order gastric emptying

| Peff | ASF | pH | Transit Time (h) | Volume (mL) | Length (cm) | Radius (cm) | SEF | Bile Salt (mM) |
|------|-------|------|------------------|-------------|-------------|-------------|-------|----------------|
| 0 | 0.0 | 4.90 | 2.45 | 978.5 | 29.19 | 9.87 | 1.000 | 0.0 |
| 0 | 2.721 | 5.40 | 0.23 | 14.57 | 14.56 | 1.56 | 4.235 | 22.28 |
| 0 | 2.668 | 5.40 | 0.94 | 166.6 | 60.26 | 1.48 | 3.949 | 18.09 |
| 0 | 2.665 | 6.00 | 0.74 | 131.0 | 60.26 | 1.32 | 3.488 | 14.99 |
| 0 | 2.640 | 6.60 | 0.58 | 102.0 | 60.26 | 1.16 | 3.029 | 10.14 |
| 0 | 2.621 | 6.90 | 0.42 | 75.35 | 60.26 | 1.00 | 2.569 | 7.093 |
| 0 | 2.589 | 7.40 | 0.29 | 53.57 | 60.26 | 0.84 | 2.109 | 1.049 |
| 0 | 0.352 | 6.40 | 4.36 | 50.49 | 13.50 | 3.45 | 1.790 | 0.0 |
| 0 | 0.823 | 6.80 | 13.07 | 53.55 | 28.35 | 2.45 | 2.480 | 0.0 |

Enzyme and Transporter Regional Distributions

C1-C4: 0.06944 0.43028 0.12147 0.4663

Fed Meal Options

Physiology: Human - Physiological - Fed

ASF Model: Opt logD Model SA/V 6.1

Percent Fluid in SI: 40 Colon: 10

Biorelevant solubilities from ADMET Predictor v6.1

pKa Table | logD: Struct-6.1 Diss Model: Johnson PartSize-Sol: ON BileSalt-Sol: ON | Diff: ON ConstRad: ON Precip: Time Ppara: OFF EHC: OFF ACAT: Cc

- Link gastric emptying time to meal calories
- Account for effect of fat content on bile salt concentration

Fed State Model

Fed State Model: Default

Meal Calories: 233.68 % Fat in Meal: 30.00

Current gastric transit time of 1.00 hr.

Current duodenum bile salt concentration is 14.44 mM.

Cancel OK

Fed State Model

Fed State Model: Default

Meal Calories: 233.68 % Fat in Meal: 30.00

Current gastric transit time of 1.00 hr.

Current duodenum bile salt concentration is 14.44 mM.

Default
User-Defined Fat and Calories
FDA Breakfast Meal
Low Fat - Low Calorie Meal
Low Fat - Moderate Calorie Meal
Low Fat - High Calorie Meal
Moderate Fat - Low Calorie Meal
Moderate Fat - Moderate Calorie Meal

Cancel OK

Predicting Proton Pump Inhibitors (PPIs) Effects

GastroPlus(TM): AZD0865-VL.mdb (C:\Doc...\Wiera1\Des...\GPv...\GP8.0\GP8...\...)

File Edit Database Simulation Setup Controlled Release Tools Modules (Optional) Help

Compound Gut Physiology-Hum Pharmacokinetics Simulation Graph

Compartmental Parameters

Hum PO 1 mpk soln. Excrete all un-absorbed drug at the end of gut transit time
 Zero-order gastric emptying

| Compartment Data | | | | | | | | | | | | | Enzyme and Transporter Regional Distributions | |
|------------------|------|-------|------|------------------|-------------|-------------|-------------|-------|----------------|------------|-----------------------------|------------|---|----------|
| Compartment | Peff | ASF | pH | Transit Time (h) | Volume (mL) | Length (cm) | Radius (cm) | SEF | Bile Salt (mM) | Pore R (Å) | Poros/L (cm ⁻¹) | Comp. Type | 3A4 Expr | 3A4 Turn |
| Stomach | 0 | 0.0 | 4.90 | 1.00 | 1000.0 | 30.00 | 10.00 | 1.000 | 0.0 | 2.200 | 2.580 | Stomach | 0.0 | 5.0E-4 |
| Duodenum | 0 | 2.630 | 5.40 | 0.25 | 48.25 | 15.00 | 1.60 | 4.235 | 14.44 | 10.41 | 48.64 | Intestinal | 2.09E-3 | 5.0E-4 |
| Jejunum 1 | 0 | 2.616 | 5.40 | 0.95 | 175.3 | 62.00 | 1.50 | 3.949 | 12.02 | 9.640 | 38.90 | Intestinal | 3.26E-3 | 5.0E-4 |
| Jejunum 2 | 0 | 2.615 | 6.00 | 0.76 | 139.9 | 62.00 | 1.34 | 3.489 | 10.46 | 8.400 | 26.09 | Intestinal | 3.26E-3 | 5.0E-4 |
| Ileum 1 | 0 | 2.594 | 6.60 | 0.59 | 108.5 | 62.00 | 1.18 | 3.029 | 7.280 | 7.160 | 16.46 | Intestinal | 1.03E-3 | 5.0E-4 |
| | | | | | | | | | 5.990 | 5.920 | 9.540 | Intestinal | 1.03E-3 | 5.0E-4 |
| | | | | | | | | | 0.730 | 4.680 | 4.896 | Intestinal | 1.03E-3 | 5.0E-4 |
| | | | | | | | | | 0.0 | 3.920 | 2.915 | Colon | 3.1E-4 | 5.0E-4 |
| | | | | | | | | | 0.0 | 3.500 | 3.220 | Colon | 3.1E-4 | 5.0E-4 |

C1-C4: 0.06944 0.43028 0.12147 0.46632 Qh (L/min): 1.4

Physiology: Human - Physiological - Fed Percent Fluid in SI: 40 Colon: 10

ASF Model: Opt logD Model SA/V 6.1

All properties are predictions from ADMET Predictor v6.0
 Changed pKa from AP value of 5.7 to 6.1 from Carlet-PharmRes-2010-27-2119-Predicting Intestinal Precipitation
 Changed log P from AP value of 2.44 to 4.2 from Carlet-PharmRes-2010-27-2119-Predicting Intestinal Precipitation
 Changed aqueous solubility from AP value of 19 ug/mL to 1.9 ug/mL at pH 8. from from Carlet-PharmRes-2010-27-2119-Predicting Intestinal Precipitation.

pKa Table | logD: Struct-6.1 | Diss Model: Wang-Flan | PartSize-Sol: ON | BileSalt-Sol: ON | Diff: ON | ConstRad: OFF | Precip: Time | Ppara: Zhim | EHC: OFF

Ability to adjust Gastric pH and, potentially, emptying allows to predict the PPIs effects

GastroPlus System Physiology Models

1. Select Species:

- Human
- Rat
- Dog
- Monkey
- Mouse
- Minipig
- Rabbit

2. For human physiologies, specify Population, Gender, Health Status and Age (pediatrics->adults)

• Population Types:

- American
- Japanese
- Chinese

• Health Status:

- Healthy
- Hepatic Impairment
- Renal Impairment
- Obesity
- Pregnancy

The screenshot shows the 'New PEAR Physiology' dialog box. The 'PEAR Inputs' section includes dropdown menus for Species (Human), Population (American), Gender (Male), and Health Status (Healthy). The Age is set to 30 years. Below these are input fields for Height [cm] (176.14), Weight [kg] (86.27), BMI [kg/m^2] (27.8063), % Body Fat (24.6), and CO [mL/s] (98.2897). The 'PEAR Outputs' section displays a table of physiological parameters:

| Name | Volume [mL] | Perfusion [mL/s] |
|-----------------|-------------|------------------|
| Hepatic Artery | 0.0000 | 8.2791 |
| Lung | 1126.9505 | 98.2897 |
| Arterial Supply | 2230.4526 | 98.2897 |
| Venous Return | 4460.9051 | 98.2897 |
| Adipose | 29285.8786 | 9.7522 |
| Muscle | 20984.5946 | 10.4923 |
| Liver | 1651.5653 | 25.2855 |
| ACAT Gut | 0.0000 | 14.0869 |
| Spleen | 175.1671 | 2.9195 |
| Heart | 326.9015 | 3.9774 |
| Brain | 1492.6488 | 12.6875 |
| Kidney | 285.7143 | 17.5237 |
| Skin | 1981.8784 | 3.9638 |
| ReproOrg | 32.4375 | 0.1135 |
| RedMarrow | 1189.6859 | 5.9484 |
| YellowMarrow | 3306.9146 | 1.6535 |
| RestOfBody | 13783.7775 | 6.8919 |

At the bottom of the outputs section, it states: Non-perfused bone [g]: 5742.353 (% BW: 6.656). The dialog box has 'OK' and 'Cancel' buttons at the bottom right.

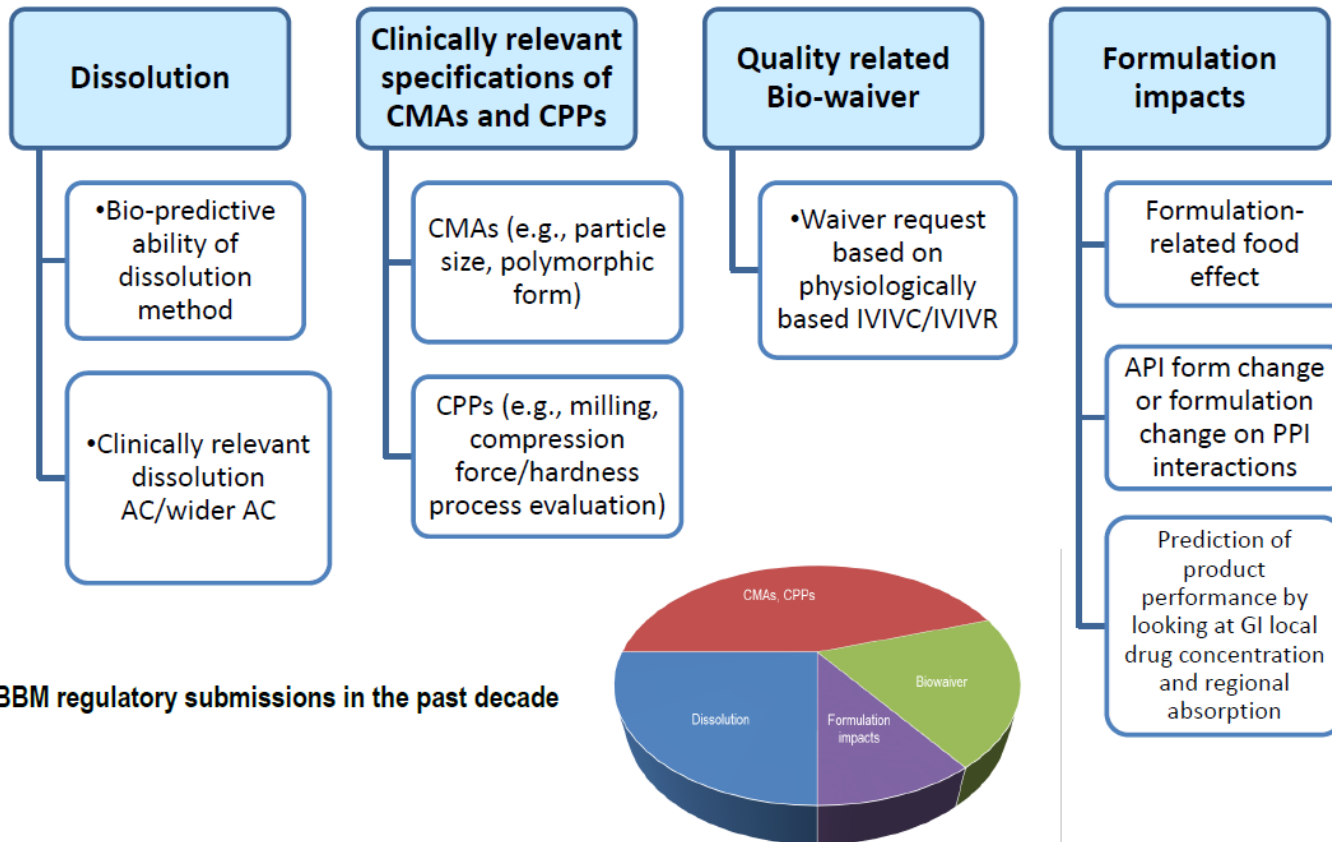
For infants specify born at term or premature infant (day 1 of birth, up to 16 weeks premature)

FDA Workshop (September 2019): Current State/Future Expectations of Translational Modeling Strategies to Support Drug Product Development, Manufacturing Changes and Controls

- **Physiologically based biopharmaceutics modeling (PBBM)**
 - Translate formulation and manufacturing changes into *in vivo* performance
 - Predict impact of variations in critical properties through establishing a ‘safe space’ via IVIVR/C combined with virtual BE trial simulations
- Today: FDA open to proposals of using PBBM approaches to establish clinically relevant product specifications
 - Proposals should include information about:
 - Modeling approach
 - Scientific justification of the proposed approach
 - Model verification

<https://cersi.umd.edu/current-state-and-future-expectations-translational-modeling-strategies-support-drug-product>

Common regulatory applications of PBBM in support of drug product quality



Best Practices for Applying PBBM to Assess Virtual Bioequivalence

- Case studies illustrate how PBBM assists with development of innovator and generic products
 - Considerations when using *in vitro* dissolution data to guide formulation simulations
 - Applying virtual BE trial simulations to help define bioequivalence and product specs

Mitra et al. Eur. J. Pharma. Biopharm. 2019

European Journal of Pharmaceutics and Biopharmaceutics 134 (2019) 117–125

Contents lists available at ScienceDirect

European Journal of Pharmaceutics and Biopharmaceutics

journal homepage: www.elsevier.com/locate/ejpb

Research paper

Physiologically based absorption modeling to predict bioequivalence of controlled release and immediate release oral products

Amitava Mitra^{a,*}, Bostjan Petek^b, Aleksander Bajc^c, Raja Velagapudi^a, Igor Legen^b

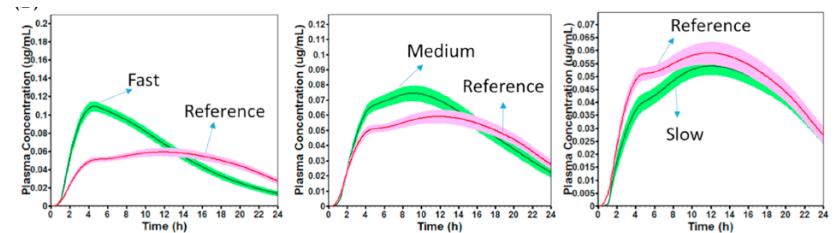
^a Clinical Development, United States
^b Dissolution Sciences, Slovenia
^c Clinical Development, Slovenia

ARTICLE INFO

Keywords:
Physiologically based pharmacokinetic (PBPK)
Absorption modeling
Bioequivalence
Controlled release
Immediate release

ABSTRACT

Physiologically based absorption modeling was conducted to predict bioequivalence (BE) for immediate release (IR) and controlled release (CR) formulations. In case of the CR formulation of a BCS class 1 drug, sensitivity analyses were conducted to investigate the impact of gastrointestinal (GI) transit time and absorption scaling factors in caecum and colon on formulation PK. The regional absorption profiles of the test and reference formulations were compared to provide additional confidence on the BE predictions. For IR formulation of BCS class 2b drug, the sensitivity of dissolution rate, precipitation time and human permeability were evaluated. Finally for both cases, population simulations were conducted in crossover manner to investigate BE between formulations, and compared with the observed data. These case studies highlight the utility of absorption modeling in prediction of BE. Such modeling can be used for development of innovator and generic products, as well as to address questions arising during regulatory reviews.



PBBM Simulations and Virtual BE to Justify Product Specifications

- Case studies illustrate how PBBM IVIVRs and virtual BE trial simulations support product specs
 - Recommendations when traditional IVIVCs cannot be developed due to lack of data
 - Applying virtual BE trial simulations to help define bioequivalence and product specs

Jereb et al. AAPS PharmSciTech 2020

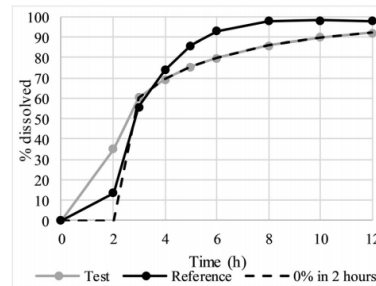


Fig. 1. Dissolution profiles of test and reference MR capsules in 500 ml 0.003% polysorbate 80 for 2 h followed by 500 mL phosphate buffer pH 7.2 for 10 h at 37°C, Apparatus 2, USP, 100 rpm with sinker. A hypothetical dissolution profile with 0% of drug dissolved in 2 h is also presented

AAPS PharmSciTech (2020) 21: 18
DOI: 10.1208/s12249-019-1566-x

Research Article

***In vitro–In vivo* Relationship and Bioequivalence Prediction for Modified-Release Capsules Based on a PBBK Absorption Model**

Rebeka Jereb,^{1,3} Jerneja Opara,² Igor Legen,² Boštjan Petek,² and Darja Grabnar-Peklar²

Received 12 June 2019; accepted 9 October 2019; published online 9 December 2019

Abstract. A physiologically based pharmacokinetic (PBBK) absorption model was developed in GastroPlus™ based on data on intravenous, immediate-release (IR), and modified-release (MR) drug products. The predictability of the model was evaluated by comparing predicted and observed plasma concentration profiles; average prediction errors (PE) were below 10%. IVIVR was developed using mechanistic deconvolution for a MR drug product to evaluate the *in vivo* effect of a proposed change in dissolution specification. The predictability of the IVIVR was evaluated and PE were below 10%; however, external validation was not possible due to the lack of data. The developed PBBK absorption model and IVIVR were used to predict plasma concentration profiles and pharmacokinetic (PK) parameters for a hypothetical formulation with 0% of drug dissolved in 2 h in *in vitro* dissolution test. Both methods predicted the insignificant effect of a change in *in vitro* dissolution profile on *in vivo* product performance. The bioequivalence of a hypothetical formulation to the test product was evaluated using virtual clinical trial. The performed analysis supported the proposed change in dissolution specification. A validated PBBK

Page 9 of 11 18

PharmSciTech (2020) 21: 18

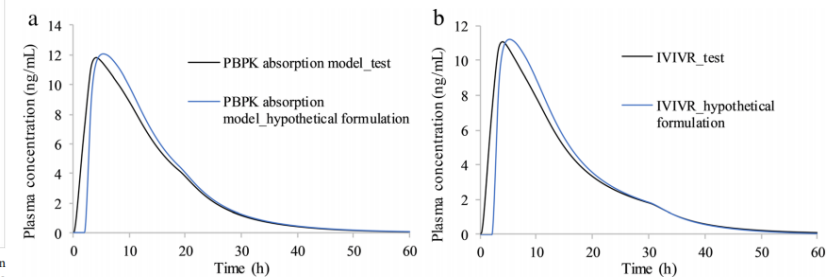


Fig. 5. Predicted mean plasma concentration profiles of a test MR formulation and a hypothetical formulation with 0% of drug dissolved in 2 h *in vitro* using **a** PBBK absorption model or **b** IVIVR equation and appropriate dissolution profiles

Food Effect Projections via Physiologically Based Pharmacokinetic Modeling: Predictive Case Studies

Criteria Supporting the Reliability of PBPK Simulation of Food Effect (FE)

- BCS/BDDCS – Class I and II
- Major mechanism for food effect is related to bile solubilization or supersaturation¹
- Linear pharmacokinetics with no significant gut transporter involvement²
- Clinical data in one prandial state available for model verification

Build First Human PBPK Model

Develop & Validate PBPK Model

1. Physicochemical properties (i.e. bio-relevant solubility and dissolution data)
2. Clinical PK after oral IR (& i.v. administration if available³)
3. Simulate with default physiological absorption model (fasted or fed) & verify vs. observed data
4. Optimize model⁴

Predict & Verify FE for Early Stage

Predict and Verify Food Effect Model

1. Apply validated human model using default fasted & fed physiologies
2. Simulate PK for non-tested prandial state
3. Predict food effect & verify vs. clinical food effect data
4. Optimize model⁴

Apply FE Model for Late Stage

Apply Food Effect Model

1. Incorporate formulation related changes in model
2. Simulate & verify model with PK data for late stage formulations⁵
3. When confidence is high, predict food effect for market formulations or re-verify vs clinical PK
4. Leverage PBPK Model to inform label

Refine Model, Build Confidence and Robustness

- Parameter sensitivity analyses
- Scenario-based simulations
- Virtual simulations

Food Effect Predictions – Select References

The AAPS Journal (© 2017)
DOI: 10.1208/s12248-017-0065-9

Research Article

The impact of gastric pH, volume, and emptying on the food effect of ziprasidone oral absorption

Steven C Sutton,^{1,4} Richard Nause,² and Kuan Gandelman³

Received 22 December 2016; accepted 23 February 2017

ABSTRACT. In a recent food effect clinical study, the authors concluded that a meal consisting of ≥500 kcal, regardless of fat content, produced the maximal bioavailability for ziprasidone. Using GastroPlus™, a commercially available pharmacokinetic simulation model, we have shown that the dietary contents of the meals should be taken into account to predict food effects for ziprasidone and perhaps other BCS class I or II compounds.

KEYWORDS: Food effects; Pharmacokinetic modeling.

Evaluating impact of gastric pH, volume, and emptying of food effect (Sutton et al., 2017)

Citation: CPT Pharmacometrics Syst. Pharmacol. (2017) 6, 747-755; doi:10.1002/psp4.12228
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ORIGINAL ARTICLE

Combining “Bottom-up” and “Top-down” Approaches to Assess the Impact of Food and Gastric pH on Pictilisib (GDC-0941) Pharmacokinetics

Tong Lu¹, Grazyna Fraczekiewicz², Laurent Salphati³, Nageshwar Budha¹, Gena Dalziel⁴, Gillian S. Smelick¹, Kari M. Morrissey¹, John D. Davis¹, Jin Y. Jin¹ and Joseph A. Ware^{1*}

Pictilisib, a weakly basic compound, is an orally administered, potent, and selective pan-inhibitor of phosphatidylinositol 3-kinases (PI3K). The aim of this study was to compare different methods in terms of their usefulness and applicability in deciphering *in vivo* delivery of nifedipine administered in modified release dosage forms. A detailed survey of publications on nifedipine pharmacokinetics was done and used to identify the magnitude of food effect. *In vitro* dissolution testing was performed under various experimental conditions. Obtained results indicate the potential for using the developed *in silico* model coupled with discriminative *in vitro* dissolution data for identification of the *in vivo* drug product behavior.

Bottom-up + Top-down approaches to assess food effect (Lu et al., 2017)

RESEARCH ARTICLE – Pharmacokinetics, Pharmacodynamics and Drug Transport and Metabolism

Utilizing Physiologically Based Pharmacokinetic Modeling to Inform Formulation and Clinical Development for a Compound with pH-Dependent Solubility

JOHN CHUNG,¹ FERNANDO ALVAREZ-NUNEZ,¹ VINCENT CHOW,² DOMINICK DAURIO,¹ JOHN DAVIS,² MICHAEL DODDS,² MAURICE EMERY,³ KEVIN LITWILER,² ANNE PACCALI,² JOANNA PENG,² BROOKE ROCK,² LARRY WIENKERS,² CHARLES YANG,¹ ZHIGANG YU,² JAN WAHLSTROM¹

¹Pharmaceutics Research and Development, Amgen, Inc., Thousand Oaks, California
²Pharmacokinetics and Drug Metabolism, Amgen, Inc., Seattle, Washington
³Clinical Pharmacology, Amgen, Inc., Thousand Oaks, California

Applying PBPK modeling to inform clinical development and assess food effects (Chung et al., 2015)

Acta Pharm. 65 (2015) 427–441
DOI: 10.1515/acph-2015-0039

Original research paper

Deciphering nifedipine *in vivo* delivery from modified release dosage forms: Identification of food effect

Identification of food effect for MR dosage forms (Ilic et al., 2015)

Accepted September 2, 2015

Keywords: absorption; disposition; pharmacokinetics; ADME; physiological model

>40

Approved drug product applications supported
by GastroPlus® simulations

Recent Approved Drug Product Applications

- ALECENSA® (**absorption/PPI DDI** informing drug labeling)
- BRAFTOVI® (**metabolism DDI** accepted by regulatory agencies)
- CALQUENCE® (**particle size specs** accepted by regulatory agencies)
- FARYDAK® (**food effect/PPI predictions** informing drug labeling)
- INLYTA® (**transporter DDI** accepted by regulatory agencies)
- KISQALI® (**gastric pH predictions** accepted by regulatory agencies)
- MEKINIST® (**transporter DDI** accepted by regulatory agencies)
- MEKTOVI® (**metabolism DDI** accepted by regulatory agencies)
- OPSUMIT® (**particle size specs** accepted by regulatory agencies)
- TAMIFLU® (**pediatric PBPK** predictions informing **dose selection**)
- ZURAMPIC® (**wider product specs** accepted by regulatory agencies)
- ... and more!

No other PBBM/PBPK platform has the diversity in applications!

Rates of Acceptance of PBPK Analysis by FDA/EMA

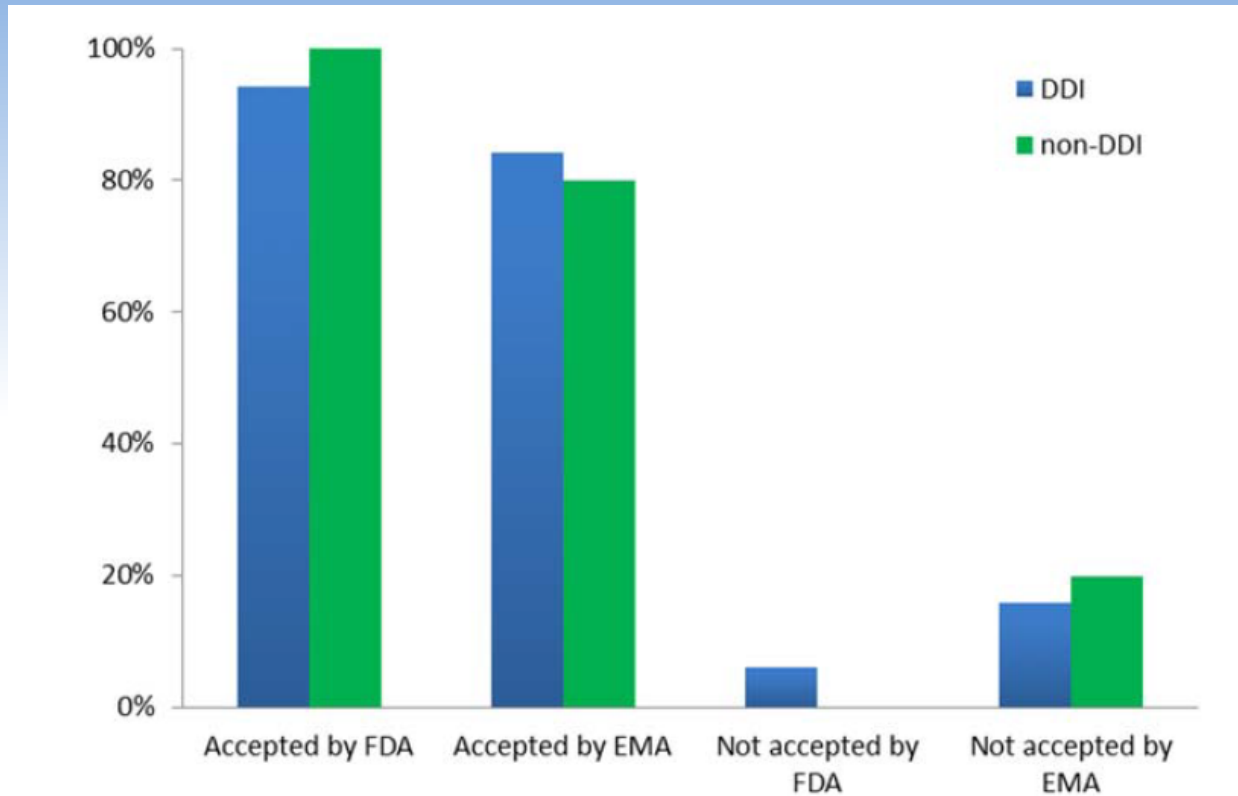


Figure 3 Rates of acceptance of PBPK analyses by the FDA or EMA among DDI and non-DDI related submissions.

PBPK Modeling Impact for Regulatory Activities in the FDA OGD (Calendar Year 2016)

| Type | No. | Examples |
|---------------------------|-----|--|
| ANDA Reviews | 20 | ❖ PD modeling and simulation for Methylphenidate ER product and asthma controllers |
| CP, CC, Pre-ANDA meetings | 54 | <ul style="list-style-type: none"> ❖ Development of BE criteria for pain killers ❖ Assessment of BE standards for GI locally acting products ❖ Simulation of in vivo alcohol dose dumping studies |
| BE Guidances | 33 | ❖ Simulations for the development of BE criteria for HVDs and NTI drugs |
| Regulatory Research Study | 37 | ❖ PK/PD modeling and simulation to determine the appropriate study design and evaluate BE between generic anti-epilepsy drugs and immunosuppressant drugs in patients |

7

ANDA: abbreviated new drug application; BE: bioequivalence; CP: citizen petition; CC: controlled correspondence; GI: gastrointestinal; HVD: highly variable drugs; NTI: narrow therapeutic index.

Highlights of PBPK Impacts (2016) at the FDA Office of Generic Drugs

| Category | Example Drug | Impact on regulatory decision making |
|--------------------------|--------------------------------------|--|
| Dissolution | Fingolimod, Oxybutynin | Risk assessment for not conducting in vivo studies for lower strength generic products when bioequivalence has been established at higher strengths |
| Product quality | Prasugrel | Conclusion that less than 20% free base in prasugrel HCl product ensures in vivo BE of the generic product including subjects on PPI |
| Mechanism change risks | Venlafaxine | Model predicted that a delayed onset of venlafaxine release up to 4 h predicted to demonstrate BE for the openable matrix release mechanism against the osmotic pump based release mechanism |
| PPI effect | Several ER products | Risk assessment of changing drug release to a PH dependent mechanism |
| PK metrics determination | Mesalamine Suppositories | Determination of PK metrics for BE evaluation |
| Alcohol dose dumping | Metformin Hydrochloride ER Tablet | Assessment of alcohol dose dumping potential |
| Virtual simulation | Methylphenidate | Assessment of using PBPK model in combination with a two way crossover study to meet the guidance recommendation of a four way crossover study for BE assessment |

PPI: proton pump inhibitor
ER: extended release

Selected FDA Publications

RESEARCH ARTICLE – Pharmacokinetics, Pharmacodynamics and Drug Transport and Metabolism

Application of Physiologically Based Absorption Modeling for Amphetamine Salts Drug Products in Generic Drug Evaluation

ANDREW H. BABISKIN, XINYUAN ZHANG

Division of Quantitative Methods and Modeling, Office of Research and Standards, Office of Generic Drugs, Center for Drug Evaluation and Research, US Food and Drug Administration, Silver Spring, Maryland 20993

Received 30 January 2015; revised 8 April 2015; accepted 9 April 2015

Using M&S to predict virtual BE and assess dissolution specifications
(Babiskin et al., 2015)

Published 2015. This article is a U.S. Government work and is in the public domain in the USA J Pharm Sci

Keywords: physiological model; absorption; bioequivalence; bioavailability; clinical trial simulation; modified release

RESEARCH PAPER

Use of In Vitro-In Vivo Correlation to Predict the Pharmacokinetics of Several Products Containing a BCS Class I Drug in Extended Release Matrices

Tahseen Mirza • Srikanth A. Byladi • Christopher D. Ellison • Yongheng Tang • Barbara M. Davit • Mansoor A. Khan

Received: 28 February 2012 / Accepted: 9 August 2012
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ABSTRACT

Purpose To determine if an IVIVC model can predict PK profiles of varying formulations of a BCS Class I drug that is a salt of a weak base.

Method An IVIVC model (Level A) was created by combining deconvoluted in vivo absorption data obtained from oral administration of 50 mg, 100 mg, and 200 mg fast and slow extended release formulations with in vitro percent dissolved using residual regression analysis. The model was then used to predict the in vivo profile of the test products that varied in formulation characteristics.

Results The model passed internal validation for predicted C_{max} and AUC. For external validation, in vitro data of five different test formulations was utilized. The model passed external validation for two test formulations that were different but belonging to the same release mechanism as that of the reference formulation. Three formulations failed external validation because they belonged to either a mixed or different release mechanism. The model and results were further confirmed

ABBREVIATIONS

| | |
|--------------------------------|---|
| AUC | area under the curve |
| BCS | biopharmaceutics classification system |
| C_{max} | maximum drug concentration observed in the blood plasma profile |
| fRA | fraction of drug absorbed into the body |
| fRD | fraction of drug dissolved during in vitro experimentation |
| IVIVC | in vitro-in vivo correlation |
| k_e | constant of elimination |
| MAPE | mean absolute percentage error |
| rpm | revolutions per minute |
| SURAC-MR | scale up post approval changes modified release |
| V_d | volume of distribution |
| %PE _{AUC} | percent error of AUC prediction |
| %PE _{C_{max}} | percent error of C_{max} prediction |

INTRODUCTION

In vitro-in vivo correlation (IVIVC) has been defined by the United States Pharmacopoeia (USP) Subcommittee on Biopharmaceutics as "the establishment of a rational relationship between a biological property, or parameter derived from a biological property produced by a dosage form, and a physicochemical property or characteristic of the same dosage form" (1). The Food and Drug Administration defines IVIVC as "A predictive mathematical model describing the relationship between an *in situ* property of an extended release dosage form (usually the rate or extent of drug dissolution or release) and a relevant *in vivo* response, e.g., plasma drug concentration or amount of drug absorbed" (2). In most cases, the *in situ* property is the rate or extent of drug dissolution or release while the *in vivo* response is the plasma drug concentration

Generating mechanistic IVIVCs to predict test formulations
(Mirza et al., 2012)

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Published online: 22 August 2012



Research Article

Utility of Physiologically Based Absorption Modeling in Implementing Quality by Design in Drug Development

Xinyuan Zhang,¹ Robert A. Lionberger,^{1,2} Barbara M. Davit,¹ and Lawrence X. Yu¹

Received 16 September 2010; accepted 14 December 2010; published online 5 January 2011

Abstract. To implement Quality by Design (QbD) in drug development, scientists need tools that link drug product properties to *in vivo* performance. Physiologically based absorption models are potentially useful tools; yet, their utility of QbD implementation has not been discussed or explored much in the literature. We simulated pharmacokinetics (PK) of carbamazepine (CBZ) after administration of four oral formulations, immediate-release (IR) suspension, IR tablet, extended-release (XR) tablet and capsule, under fasted and fed conditions and presented a general diagram of a modeling and simulation strategy integrated with pharmaceutical development. We obtained PK parameters and absorption scale

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Incorporating M&S to assist with Quality by Design (QbD)
(Zhang et al., 2011)

KEY WORDS: advanced compartmental absorption and transit (ACAT) model; gastroplus™; modified release (MR); quality by design (QbD).

Integrating in vitro, modeling, and in vivo approaches to investigate warfarin bioequivalence

Xinyuan Zhang^{1,*}, Hong Wen^{1,*}, Jianghong Fan^{1,*}, Bradley Vince², Tonglei Li³, Wei Gao³, Minoru Kinjo^{1,*}, Jill Brown^{4,*}, Wanjie Sun^{4,*}, Wenlei Jiang^{1,*}, and Robert Lionberger^{1,*}

Virtual BE trial simulations for warfarin
(Zhang et al., 2017)

¹ Office of Generic Drugs, Food and Drug Administration, Silver Spring, MD

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³ Department of Industrial and Physical Pharmacy, Purdue University, West Lafayette, IN

⁴ Office of Translational Sciences, Food and Drug Administration, Silver Spring, MD

Case Study: Crossover Trials to Show BE after Manufacturing Changes

M&S Objectives

- Post approval, sponsor's manufacturing process change resulted in different particle size distributions for new lots
 - Inline milling step added to crystallization process (PE)
- With GastroPlus, could they apply for a biowaiver by:
 - assessing the effects of changes in particle size distribution of the active pharmaceutical ingredient (API) on its oral bioavailability?
 - predicting the virtual bioequivalence between the “new” and “old” API lots?

Proposed Modeling Tasks

- Part I: determine the most appropriate absorption/PBPK model for the API across several doses for the non-engineered lots
- Part II: assess the effect of particle size on API exposure for the immediate release formulation
- Part III: evaluate predicted bioequivalence of the tablets manufactured with particle-engineered (PE) API (narrower particle size distribution) versus the tablets manufactured with non particle-engineered (NPE) API (broader particle size distribution)

Part I: Building the Baseline Model: Key Modeling Parameters

- **Canagliflozin** - BCS Class IV drug
- Neutral compound
- Aqueous solubility = 10 µg/mL
- Significant solubilization by bile salts
- Intermediate lipophilicity
- No food effect

Various Particle Size Used in Clinical Studies

| NPE API Lot Number | d10 (µm) | d50 (µm) | d90 (µm) | PE API Lot Number | d10 (µm) | d50 (µm) | d90 (µm) |
|--------------------|----------|----------|----------|-------------------|----------|----------|----------|
| NPE Lot 1 | 20 | 63 | 173 | PE Lot 1 | 16 | 40 | 88 |
| NPE Lot 2 | 8 | 179 | 512 | PE Lot 2 | 20 | 49 | 102 |
| NPE Lot 3 | 15 | 49 | 142 | PE Lot 3 | 22 | 53 | 108 |
| NPE Lot 4 | 31 | 86 | 348 | PE Lot 4 | 19 | 39 | 71 |
| NPE Lot 5 | 26 | 78 | 276 | PE Lot 5 | 17 | 35 | 67 |
| NPE Lot 6 | 9 | 29 | 101 | PE Lot 6 | 23 | 48 | 93 |
| NPE Lot 7 | 11 | 35 | 114 | PE Lot 7 | 21 | 44 | 87 |
| NPE Lot 8 | 12 | 37 | 124 | PE Lot 8 | 21 | 45 | 90 |
| NPE Lot 9 | 10 | 36 | 119 | PE Lot 9 | 24 | 50 | 94 |
| NPE Lot 10 | 13 | 45 | 138 | PE Lot 10 | 21 | 45 | 89 |
| NPE Lot 11 | 11 | 35 | 99 | PE Lot 11 | 19 | 42 | 88 |
| | | | | PE Lot 12 | 22 | 47 | 95 |

API: active pharmaceutical ingredient; d10, d50, and d90: diameter for which 10%, 50%, and 90% (respectively) by volume of the particles are less than this value; NPE: non-particle-engineered; PE: particle-engineered

Compound: Propranolol HCl

Reset All Values Excrete all un-absorbed drug at the end of gut transit time
 Zero-order gastric emptying

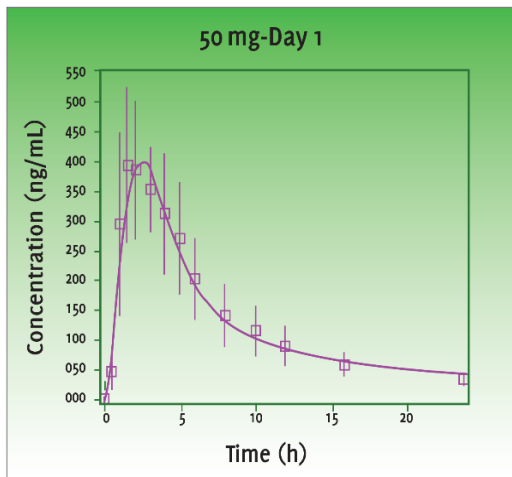
| Compartment | Peff | ASF | pH | Transit Time (h) | Volume (mL) | Length (cm) | Radius (cm) | SEF | Bile Salt (mM) |
|-------------|------|-------|------|------------------|-------------|-------------|-------------|-------|----------------|
| Stomach | 0 | 0.0 | 1.30 | 0.25 | 48.92 | 29.19 | 9.87 | 1.000 | 0.0 |
| Duodenum | 0 | 2.727 | 6.00 | 0.26 | 44.57 | 14.58 | 1.56 | 4.235 | 2.800 |
| Jejunum 1 | 0 | 2.678 | 6.20 | 0.94 | 166.6 | 60.26 | 1.48 | 3.949 | 2.330 |
| Jejunum 2 | 0 | 2.675 | 6.40 | 0.74 | 131.0 | 60.26 | 1.32 | 3.489 | 2.030 |
| Ileum 1 | 0 | 2.640 | 6.60 | 0.58 | 102.0 | 60.26 | 1.16 | 3.029 | 1.410 |
| Ileum 2 | 0 | 2.621 | 6.90 | 0.42 | 75.35 | 60.26 | 1.00 | 2.569 | 1.160 |
| Ileum 3 | 0 | 2.589 | 7.40 | 0.29 | 53.57 | 60.26 | 0.84 | 2.109 | 0.140 |
| Caecum | 0 | 0.352 | 6.40 | 4.36 | 50.49 | 13.50 | 3.45 | 1.790 | 0.0 |
| Asc. Colon | 0 | 0.823 | 6.80 | 13.07 | 53.55 | 28.35 | 2.45 | 2.480 | 0.0 |

C1-C4: [0.06944] [0.43028] [0.12147] [0.46632] Qh (L/min): [1.5]

Physiology: Human - Physiological - Fasted Percent Fluid in St: [40] Colon: [10]

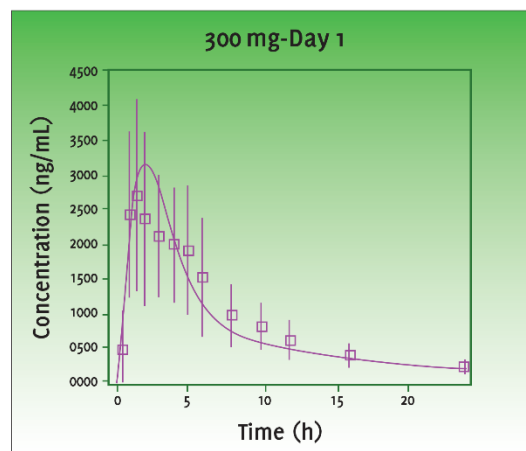
ASF Model: [Dpt logD Model SA/V 6.1]

Part I: Simulation Results for Baseline Models of Non-Engineered Lots



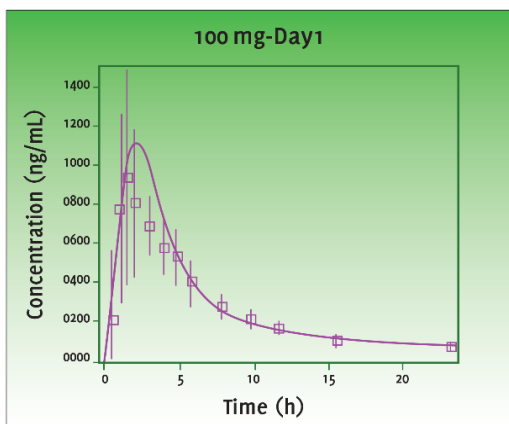
Total simulation time (h): 24

| Result | Observ | Simul |
|---------------------|--------|--------|
| Fa (%) | 0 | 85.907 |
| FD _p (%) | 0 | 85.907 |
| F (%) ₀ | 0 | 71.303 |
| Cmax (ng/mL): | 391.2 | 399.12 |
| Tmax (h): | 1.5 | 2.56 |
| AUC o-inf (ng-h/mL) | 3563.7 | 3739.6 |
| AUC o-t (ng-h/mL): | 3139.1 | 3702 |
| Cmax Liver (ng/mL): | | 531.85 |



Total simulation time (h): 24

| Result | Observ | Simul |
|---------------------|--------|--------|
| Fa (%) | 0 | 96.422 |
| FD _p (%) | 0 | 96.422 |
| F (%) ₀ | 0 | 80.03 |
| Cmax (ng/mL): | 2768 | 3245.8 |
| Tmax (h): | 1.5 | 2.08 |
| AUC o-inf (ng-h/mL) | 26290 | 24970 |
| AUC o-t (ng-h/mL): | 22590 | 20990 |
| Cmax Liver (ng/mL): | | 4079.7 |

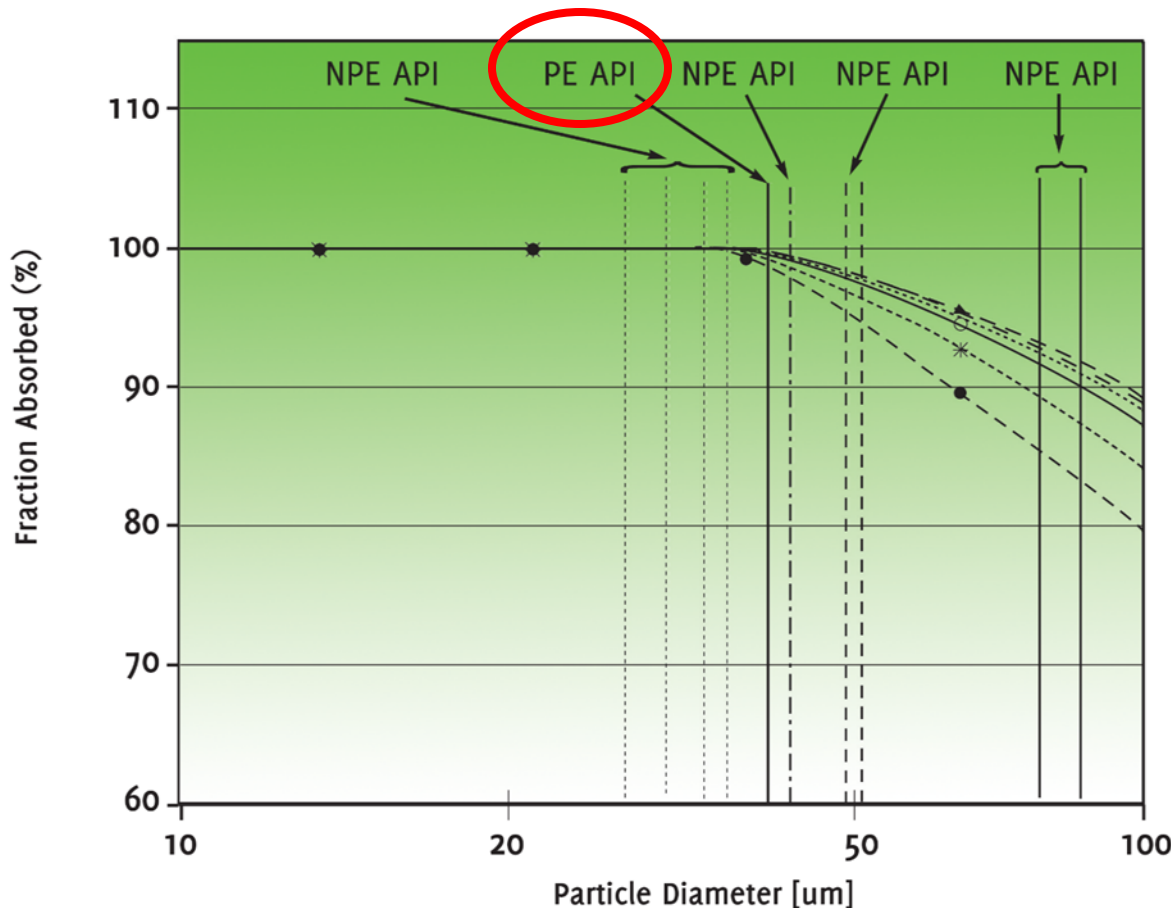


Total simulation time (h): 24

| Result | Observ | Simul |
|---------------------|--------|--------|
| Fa (%) | 0 | 85.907 |
| FD _p (%) | 0 | 85.907 |
| F (%) ₀ | 0 | 71.303 |
| Cmax (ng/mL): | 926.3 | 399.12 |
| Tmax (h): | 1.5 | 2.56 |
| AUC o-inf (ng-h/mL) | 7545.6 | 8462.2 |
| AUC o-t (ng-h/mL): | 6358.8 | 7117.3 |
| Cmax Liver (ng/mL): | | 1385.9 |

Same baseline absorption model does a good job of predicting the observed plasma concentration-time data across the three different doses of the NPE (“old”) API lots.

Part II: Parameter Sensitivity Analysis (PSA) Around Mean Particle Radius: Dose Range: 10 – 1000 mg



- ▲ 10 mg
- △ 20 mg
- ◆ 50 mg
- ◇ 100 mg
- 200 mg
- * 500 mg
- 1000 mg

PSA was used to establish particle size specifications.

Results indicated that there would be small changes in Fa% until the largest particle sizes of the NPE API lots (> 30 - 40 μm) were reached *and* the dose exceeded 100 mg.

Part III: Virtual Bioequivalence Trials: Population Simulator

- Incorporate measured variability for physicochemical, formulation and PK parameters into Population Simulator
- Capture observed variability from existing clinical PK studies

Population Simulator

File

Parameters

Clear All

Add All

Add Select

Set Defaults

Population

Set PEAR

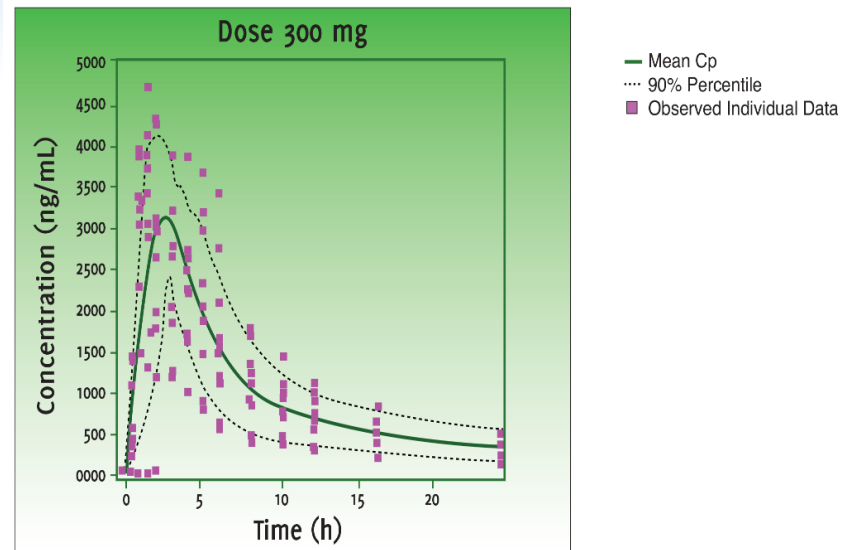
Load Previous

Create New

| Parameter | Lower Limit | Mean Value | Upper Limit | CV% | Distribution |
|---|-------------|------------|-------------|-----|--------------|
| Dose of Valsartan (mg) | 91.514 | 100 | 109.27 | 3 | log-Normal |
| Primary Permeability of Valsartan (cm) | 0.2048 | 0.92 | 4.1328 | 65 | log-Normal |
| Particle Shape Factor of Valsartan | 0.7513 | 1 | 1.331 | 10 | log-Normal |
| Mean Drug Particle Radius of Valsartan (nm) | 18.783 | 25 | 33.275 | 10 | log-Normal |
| Precipitation Particle Radius of Valsartan (nm) | 0.7513 | 1 | 1.331 | 10 | log-Normal |
| Precipitation Time of Valsartan (sec) | 676.18 | 900 | 1197.9 | 10 | log-Normal |
| Reference Solubility of Valsartan (mg/mL) | 0.0738 | 0.0982 | 0.1307 | 10 | log-Normal |
| Fraction Unbound in Enterocytes (f _u) | 0.7513 | 1 | 1.331 | 10 | log-Normal |
| Oral Transit Time of Valsartan (h) | 0.1878 | 0.25 | 0.3328 | 10 | log-Normal |
| Oral Cavity ASF Valsartan | 0.7513 | 1 | 1.331 | 10 | log-Normal |
| Duodenum ASF Valsartan | 2.1011 | 2.7965 | 3.7221 | 10 | log-Normal |
| Jejunum 1 ASF Valsartan | 2.0672 | 2.7514 | 3.6621 | 10 | log-Normal |
| Jejunum 2 ASF Valsartan | 2.0506 | 2.7294 | 3.6328 | 10 | log-Normal |
| Ileum 1 ASF Valsartan | 2.0273 | 2.6983 | 3.5914 | 10 | log-Normal |
| Ileum 2 ASF Valsartan | 1.988 | 2.6461 | 3.522 | 10 | log-Normal |
| Ileum 3 ASF Valsartan | 1.9416 | 2.5843 | 3.4396 | 10 | log-Normal |
| Caecum ASF Valsartan | 0.0797 | 0.1061 | 0.1412 | 10 | log-Normal |
| Asc. Colon ASF Valsartan | 0.1551 | 0.2064 | 0.2747 | 10 | log-Normal |
| OralMucosaVolume (mL) | 2.6296 | 3.5 | 4.6585 | 10 | log-Normal |
| SalivaProductionRate (mL/min) | 0.7513 | 1 | 1.331 | 10 | log-Normal |
| Fraction of colon fluid volume in fasted | 7.5131 | 10 | 13.31 | 10 | log-Normal |
| Fraction of SI fluid volume in fasted | 30.053 | 40 | 53.24 | 10 | log-Normal |
| Small Intestine Length (cm) | 230.01 | 306.14 | 407.47 | 10 | log-Normal |
| Caecum Length (cm) | 9.9118 | 13.193 | 17.559 | 10 | log-Normal |
| Colon Length (cm) | 20.772 | 27.648 | 36.799 | 10 | log-Normal |
| Stomach Volume (mL) | 34.981 | 46.56 | 61.972 | 10 | log-Normal |
| Small Intestine Radius (cm) | 0.7513 | 1 | 1.331 | 10 | log-Normal |
| Caecum Radius (cm) | 2.5433 | 3.3851 | 4.5056 | 10 | log-Normal |
| Colon Radius (cm) | 1.8086 | 2.4073 | 3.2041 | 10 | log-Normal |
| Stomach Transit Time (h) | 0.1447 | 0.25 | 0.432 | 20 | log-Normal |
| Small Intestine Transit Time (h) | 1.857 | 3.2088 | 5.5448 | 20 | log-Normal |

Number of Output Data Points: 300

OK Cancel



Virtual Bioequivalence Study Simulations

| API Lot | PE/NPE | Dose (mg) | AUC _∞ (ng.h/mL) (N=250) | | C _{max} (ng/mL) (N=250) | |
|---------|--------|-----------|---------------------------------------|-------------------------|-------------------------------------|-------------------------|
| | | | GM | GMR (90% CI) | GM | GMR (90% CI) |
| Lot 5 | PE | 50 | 4180 | 113.3 (110.7, 116.1) | 551 | 139.3 (136.0, 142.7) |
| Lot 1 | NPE | 50 | 3688 | | 395 | |
| Lot 5 | PE | 100 | 8242 | 103.0 (100.9, 105.1) | 551 | 106.4 (104.3, 108.6) |
| Lot 3 | NPE | 100 | 8001 | | 395 | |
| Lot 5 | PE | 300 | 24998 | 102.2 (99.8, 104.6) | 3118 | 100.0 (97.7, 102.4) |
| Lot 2 | NPE | 300 | 24460 | | 3117 | |
| Lot 5 | PE | 100 | 8242 | 98.2 (96.2, 100.2) | 1068 | 95.1 (93.2, 97.0) |
| Lot 4 | NPE | 100 | 8395 | | 1123 | |
| Lot 5 | PE | 300 | 24998 | 101.9 (99.8, 104.1) | 3118 | 98.3 (96.3, 100.4) |
| Lot 4 | NPE | 300 | 24525 | | 3171 | |



API: active pharmaceutical ingredient; AUC_∞: area under the plasma concentration-time curve from time 0 to infinite time; CI: confidence interval; C_{max}: maximum observed plasma concentration; GM: geometric mean; GMR: geometric mean ration; NPE: non-particle-engineered; PE: particle-engineered

Summary

- A mechanistic, physiologically-based absorption/PK model was constructed in GastroPlus and validated across three dose levels (50, 100, and 300 mg) using *in vivo* data collected from tablets manufactured with non particle-engineered API.
- Parameter sensitivity analysis showed that mean particle size would be the main property that determines whether formulations are likely to be bioequivalent, regardless of dose.
- Virtual bioequivalence trial simulations showed that, for a sufficiently powered study, the population-derived C_{\max} and AUC values would be bioequivalent between the tablets manufactured with non particle-engineered (NPE) vs. new particle-engineered (PE) API, up to 40 μm particle size, regardless of the dose.
- **Regulatory agencies approved the sponsor's biowaiver application**
- **Sponsor got to market ~12 months before it would have running the full trials**

Case Study: Justification of Drug Product Dissolution Rate

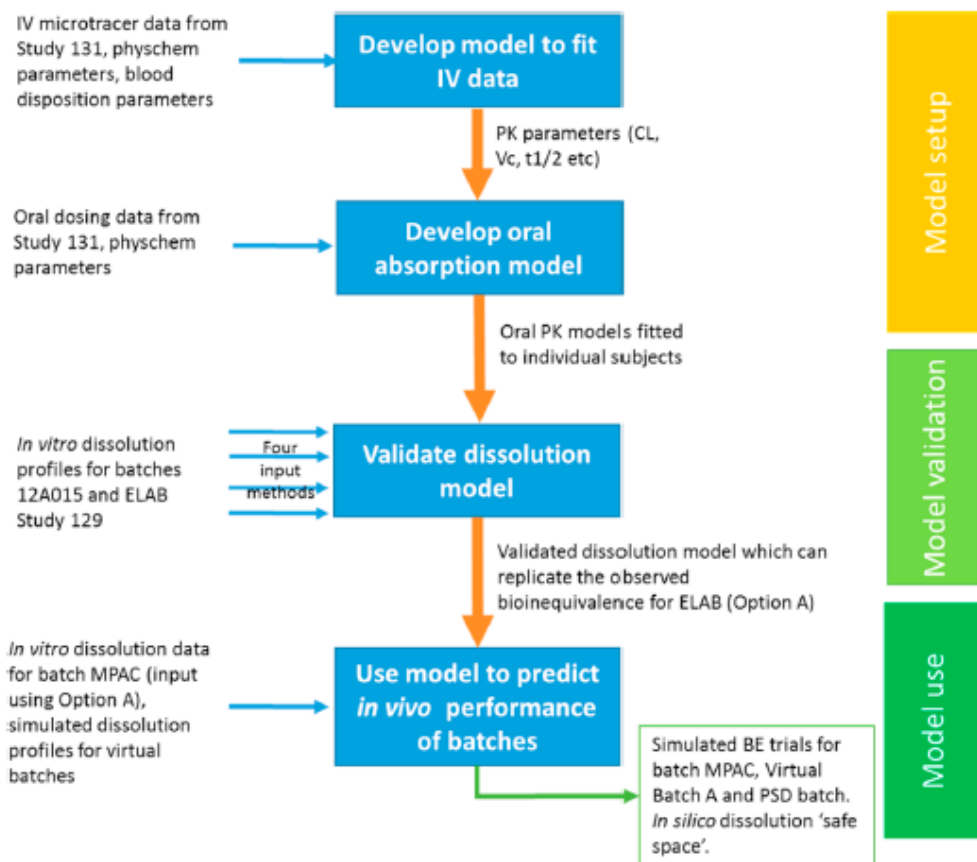
Justification of Drug Product Dissolution Rate and Drug Substance Particle Size Specifications Based on Absorption PBPK Modeling for Lesinurad Immediate Release Tablets

Xavier J. H. Pepin,^{*,†} Talia R. Flanagan,[†] David J. Holt,[†] Anna Eidelman,[‡] Don Treacy,[‡] and Colin E. Rowlings[‡]

[†]AstraZeneca, Global Medicines Development, Pharmaceutical Development, Silk Road Business Park, Charter Way, Hurdsfield Industrial Estate, Macclesfield, SK10 2NA, U.K.

[‡]Ardea Biosciences, Pharmaceutical Sciences, 9390 Towne Centre Drive, San Diego, California 92121, United States

DOI: 10.1021/acs.molpharmaceut.6b00497
Mol. Pharmaceutics 2016, 13, 3256–3269



Theoretical particle size distribution was fitted to *in vitro* dissolution data and used as an input for *in vivo* simulation

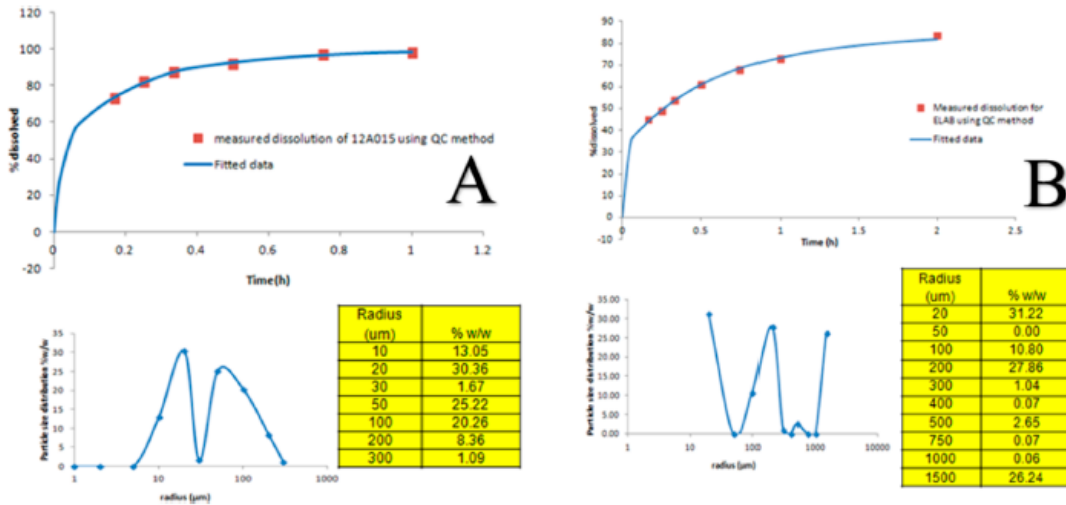


Figure 4. Fitting of dissolution profile for batch 12A015 (A) and ELAB (B) in the QC dissolution method with a theoretical particle size distribution. Note: the value presented at the 2 h time point for batch ELAB is from an infinity spin (15 min, 250 rpm).

The *in vitro* dissolution profiles showed multi-phasic behavior for these formulation and could not be successfully fitted with single z-factor.

Fitting “artificial” particle size distribution allowed for more accurate translation of *in vitro* dissolution to *in vivo*

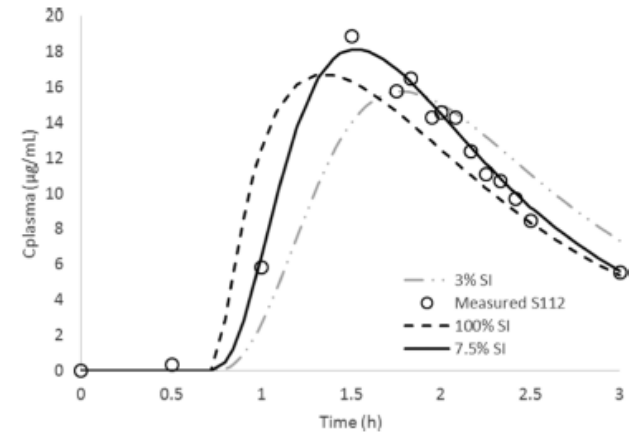


Figure 7. Simulated PK profile vs measured plasma concentrations for S112 following administration of 400 mg 12A015 tablet using Option A.

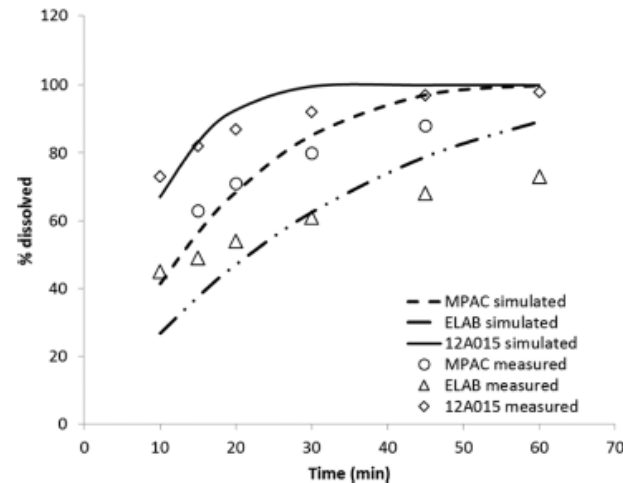
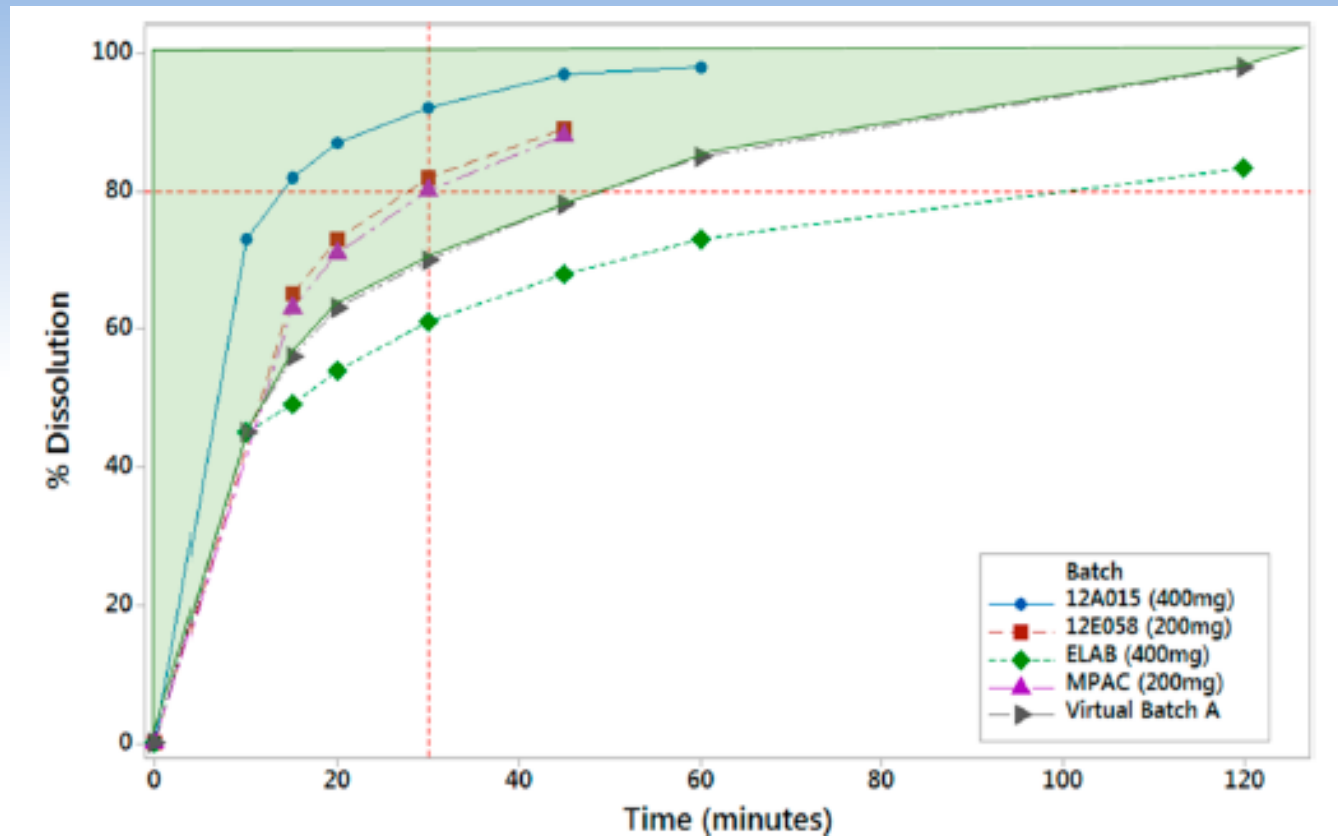


Figure 8. Z-factor fit for batches 12A015 ($Z = 1 \times 10^{-3}$ mL/mg/s), ELAB ($Z = 3.74 \times 10^{-4}$ mL/mg/s), and MPAC ($Z = 5e-4$ mL/mg/s).

Once validated, the approach was used to determine the dissolution specifications for the formulation



Other Recent Examples: Product Changes & Virtual BE

Mitra et al., AAPS PharmSciTech
2015, 16(1):76

Yanez et al., SOT Annual Meeting
2015, San Diego, CA

AAPS PharmSciTech, Vol. 16, No. 1, February 2015 (© 2014)
DOI: 10.12806/1229-014-0194-S

Research Article

Theme: Leveraging BCS Classification and *in-silico* Modeling for Product Development
Guest Editors: Divyakant Desai, John Criscon, and Peter Timmins

Application of Absorption Modeling to Predict Bioequivalence Outcome of Two Batches of Etoricoxib Tablets

Amitava Mitra,^{1,3} Filippos Kessoglou,¹ and Peter Dogterom²

Received 24 January 2014; accepted 7 August 2014; published online 3 September 2014

Abstract. As part of the overall product development and manufacturing strategy, pharmaceutical companies routinely change formulation and manufacturing site. Depending on the type and level of change and the BCS class of the molecule, dissolution data and/or bioequivalence (BE) may be needed to support the change for immediate release dosage forms. In this report, we demonstrate that for certain weakly basic low-solubility molecules which rapidly dissolve in the stomach, absorption modeling could be used to justify a BE study waiver even when there is failure to show dissolution similarity under some conditions. The development of an absorption model for etoricoxib is described here, which was then used to *a priori* predict the BE outcome of tablet batches manufactured at two sites. Dissolution studies in 0.01 N HCl media (pH 2.0) had demonstrated similarity of etoricoxib tablets manufactured at two different sites. However, dissolution testing at pH 4.5 and pH 6.8 media failed to show comparability of the tablets manufactured at the two sites. Single simulations and virtual trials conducted using the 0.01 N HCl dissolution showed similarity in AUC and C_{max} for all tablet strengths for batches manufactured at the two manufacturing sites. These predicted results were verified in a definitive bioequivalence study, which showed that both tablet batches were bioequivalent. Since the development of traditional *in vitro-in vivo* correlations (IVIVC) for immediate release (IR) products is challenging, in cases such as etoricoxib, absorption modeling could be used as an alternative to support waiver of a BE study.

KEY WORDS: bioequivalence; dissolution; modeling; pharmacokinetics; SUPAC.

RESEARCH ARTICLE – Pharmacokinetics, Pharmacodynamics and Drug Transport and Metabolism

Application of Physiologically Based Absorption Modeling for Amphetamine Salts Drug Products in Generic Drug Evaluation

ANDREW H. BABISKIN, XINYUAN ZHANG


Division of Quantitative Methods and Modeling, Office of Research and Standards, Office of Generic Drugs, Center for Drug Evaluation and Research, US Food and Drug Administration, Silver Spring, Maryland 20993

Received 30 January 2015; revised 8 April 2015; accepted 9 April 2015

Published online in Wiley Online Library (wileyonlinelibrary.com). DOI 10.1002/jps.24474

ABSTRACT: Amphetamine (AMP) salts-based extended-release (ER) drug products are widely used for the treatment of attention deficit hyperactivity disorder. We developed physiologically based absorption models for mixed AMP salts ER capsules and dextroamphetamine sulfate ER capsules to address specific questions raised during generic drug postmarketing surveillance and bioequivalence (BE) guidance development. The models were verified against several data sets. Virtual BE simulations were conducted to assess BE in various populations other than normal healthy subjects where BE studies are generally conducted for approval. The models were also used to predict pharmacokinetics (PK) for hypothetical formulations having dissolution profiles falling within specification after the development of *in vitro-in vivo* relation. Finally, we demonstrated how to use the models to test sensitivity of PK metrics to the changes in formulation variables. Published 2015. This article is a U.S. Government work and is in the public domain in the USA | Pharm Sci
Keywords: physiological model; absorption; bioequivalence; bioavailability; clinical trial simulation; modified release

Babiskin et al., J. Pharm. Sci.
2015, 104(9):3170



In-Silico Modeling: Assessing the Impact of Different Dissolution Profiles in Doxycycline Tablets (Ronaxan®): An Alternative Approach to Replace In Vivo Bioequivalence Studies for Regulatory Product Variations

Jaime A. Yañez, James Fischer, Laura Letendre and James Gerhart
Meril Inc., a Sanofi company – Drug Safety and Disposition / Pharmacokinetics and Drug Metabolism

Abstract
Final ID #
2091

Status and Problem

- Doxycycline, a tetracycline antibiotic, is approved as Ronaxan® (20, 100 and 250 mg tablets) in the EU for the treatment of respiratory tract infections in dogs.
- Changes proposed to the composition and manufacturing procedures resulted in different label dissolution profiles (within the first 15 minutes). Because a shift in the dissolution profile could impact the safety or efficacy of Ronaxan, a GastroPlus™ compartmental model was built to predict the change in kinetic parameters resulting from the proposed manufacturing changes.
- The results helped the project team to obtain regulatory approval of the variation without the need to demonstrate *in vivo* bioequivalence.

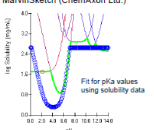
Modeling Approach

- The model was built for the dog using physicochemical properties, solubility data, IV (10 mg/kg) and oral (10 mg/kg) plasma pharmacokinetic profiles, and the dissolution profiles.
- Mechanistic homogeneous precipitation, Adson paracellular permeability and Z-factor (Takano) dissolution models were incorporated into a Beagle Fed compartmental model.
- Solubility and pKa values were adjusted based on experimental data, and a Z-factor was estimated for each dissolution profile.

Results

Model in GastroPlus (Simulation Plus, Inc.)

- **Dosage form:** Immediate release (IR) tablets
- **Species / Physiology:** Beagle dog / Fed
- **Solubility data:** Modeled using MarvinSketch (ChemAxon Ltd.)




Fit for pKa values using solubility data

IV data (10 mg/kg) Gutiérrez et al., 2012

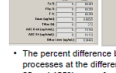
| Parameter | Value | CV% (n=6) |
|----------------------------|-------|-----------|
| $t_{1/2}$ (h) | 20.0 | 8.0 |
| $t_{1/2}$ (h) | 10.0 | 8.0 |
| CL _{CR} (L/h) | 0.400 | 8.0 |
| V_d (L) | 10.0 | 8.0 |
| $AUC_{0-\infty}$ (ug·h/mL) | 1700 | 8.0 |
| C_{max} (ug/mL) | 100 | 7.4 |

Modeling Results for a Change in Manufacturing Processes

Original



Updated



- The dissolution profile from each formulation (original and updated) at the dose levels: 20, 100 or 250 mg was fitted to a Z-factor (Takano) model to estimate its own Z-factor
- Next, each formulation after oral administration was simulated using the PK parameters from the IV administration.
- PK parameters (C_{max} and $AUC_{0-\infty}$) were then compared to estimate the relative % difference between original and updated manufacturing processes.
- The percent difference between tablets of the original and updated manufacturing processes at the different doses were found to be less than 3%, which was within the 80 and 125% range for bioequivalent tablets.

| Parameter | 20mg | 100mg | 250mg |
|----------------------------|-------|-------|--------|
| C_{max} (ug/mL) | 2.62% | 1.84% | 0.930% |
| $AUC_{0-\infty}$ (ug·h/mL) | 2.98% | 2.02% | 0.921% |

- **IV data:** Fit in PKPlus to a 3-compartmental model (results with graph)
- **Dissolution:** Z-Factor (Takano) model, each dissolution profile was fit to estimate its own Z-factor (Takano et al., 2008)
- **Precipitation:** Mechanistic, Homogeneous
- **Permeability:** Adson, Paracellular permeability

Virtual population pharmacokinetic using physiologically based pharmacokinetic model for evaluating bioequivalence of oral lacidipine formulations in dogs

Bin Yang¹, Chunman Wu¹, Bin Ji¹, Minghui Wu¹, Zhonggui He¹, Lei Shang^{4,6} and Jin Sun^{1,3,*}

Affiliation:

Yang et al., Asian J. Pharm. Sci.

2016; Mar 21

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²Department of Pharmacy, Tianjin Medical University Cancer Institute and Hospital, China;

³Department of Pharmaceutical analysis, School of Pharmacy, Shenyang Pharmaceutical University, China;

⁴School of Pharmacy, China Medical University, China;

⁵Municipal Key Laboratory of Biopharmaceutics, School of Pharmacy, Shenyang Pharmaceutical University, China;

Bioequivalence of Complex Generic Products

For locally acting drugs (LADs) such as dermatological, ocular, and inhalation products, clinical endpoint bioequivalence (CEBE) studies are often recommended instead of standard PK BE studies. However, many clinical endpoints are not sensitive in reflecting formulation-related differences in drug delivery to the site of action for LADs. This leads to large CEBE studies with potentially false conclusion of BE between two products.

PBBM/PBPK modeling and simulation is a tool to address bioequivalence-related challenges associated with alternative routes of delivery, such as ocular, nasal-pulmonary, and transdermal.

[Clin Pharmacol Ther.](#) 2019 Feb;105(2):295-297. doi: 10.1002/cpt.1244. Epub 2018 Nov 19.

Clinical Endpoint Bioequivalence Studies Are Not Sensitive: A Perspective From Generic Drugs.

Novakovic J¹, Szirtes J¹, Fields A¹, Tsang YC¹.

Conclusions

Evolving relationship between *in silico* tools and R&D

- **Model “supported” (first questions 20 years ago):** Do you think modeling and simulation might help?
- **Model “based” (current questions today):** How can I maximize the value of modeling and simulation in my development program?
- **Model “driven” (future questions):** How do I change the R&D process to reflect the availability of *in silico* tools and techniques?

How PBBM modeling & simulation can save resources in R&D

- Prioritize experiments to be done – **better invest resources**
- Integrate the wide variety of data obtained from *in silico*, *in vitro* and *in vivo* experiments to **tell a compelling story**
- **Reduce regulatory burden**
- Productivity tools – be the **first to market**



Additional Slides

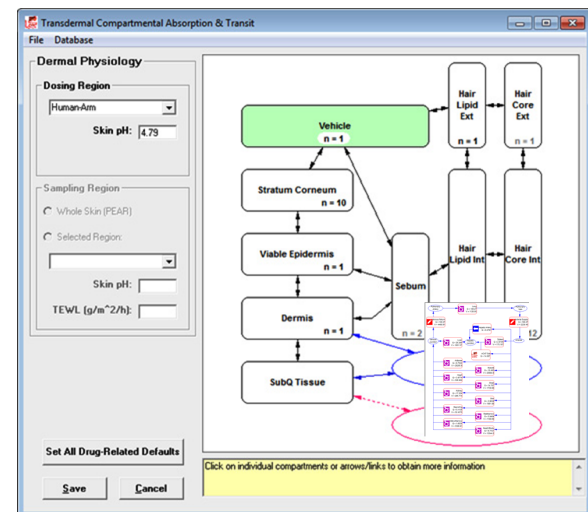
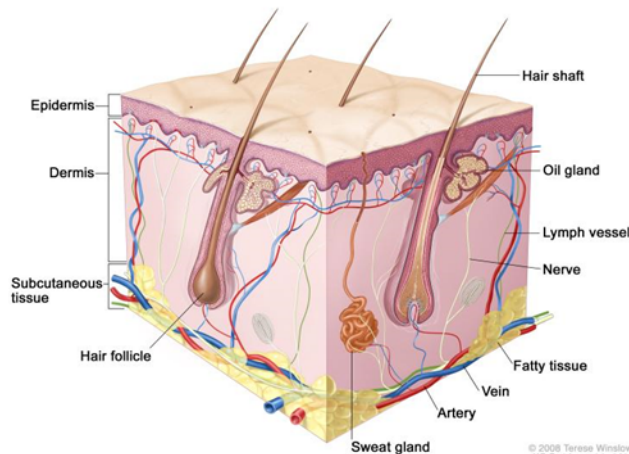
Some of Our International Pharma Customers (total > 250)



Regulatory Interactions & Collaborations

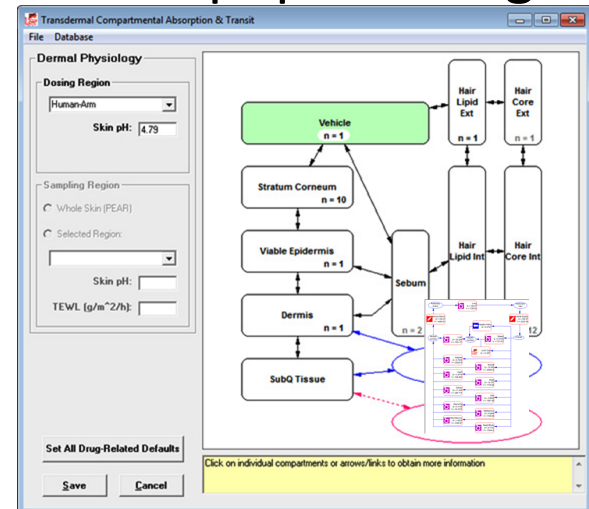
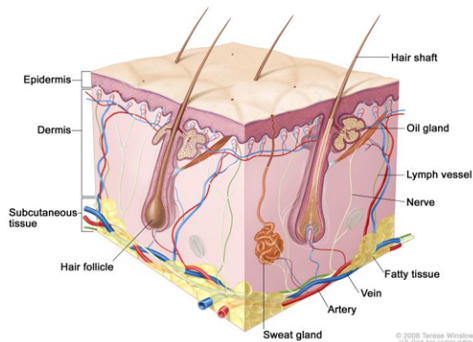
Cooperation Grant with Cosmetics Europe (2018-20)

- 1-year *funded* collaborative project with Cosmetics Europe on the enhancement & validation of GastroPlus mechanistic dermal models:
 - Compound evaporation kinetics
 - Improved partition coefficient predictions
 - Saturable metabolism kinetics within the skin



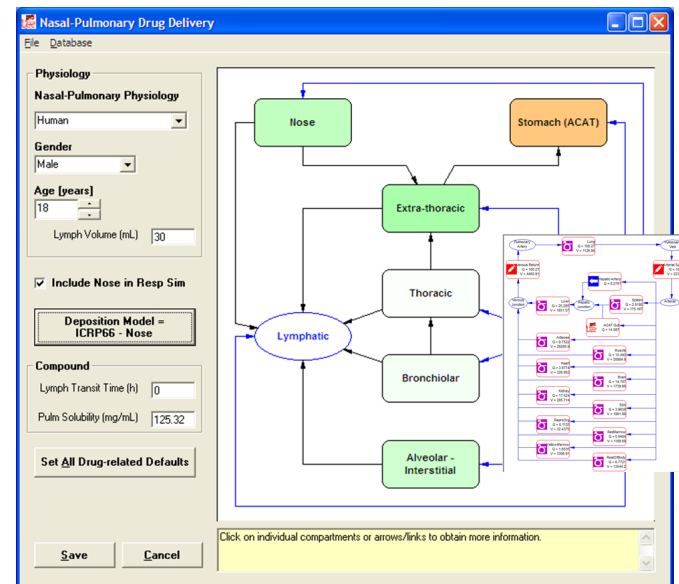
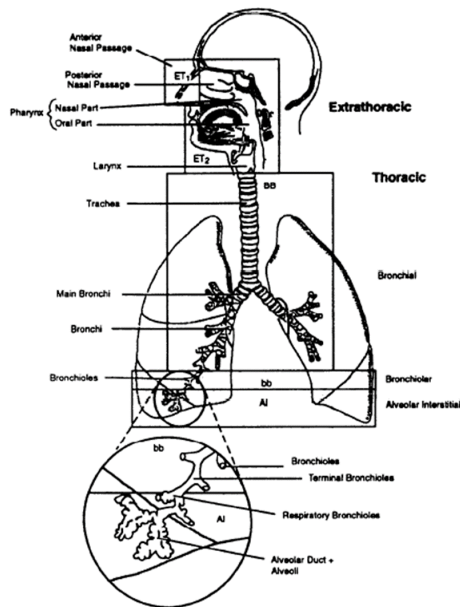
Cooperation Grant with the FDA (2018-20)

- 2-year funded collaborative project with the FDA Office of Generic Drugs on the incorporation of drug product quality attributes into the GastroPlus mechanistic dermal models:
 - Develop mechanistic equations describing *in vitro* release/permeability assays for topical formulations
 - Develop models for various APIs in different population groups



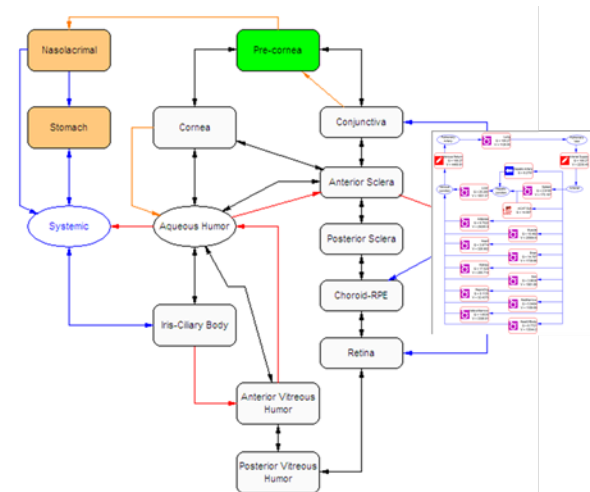
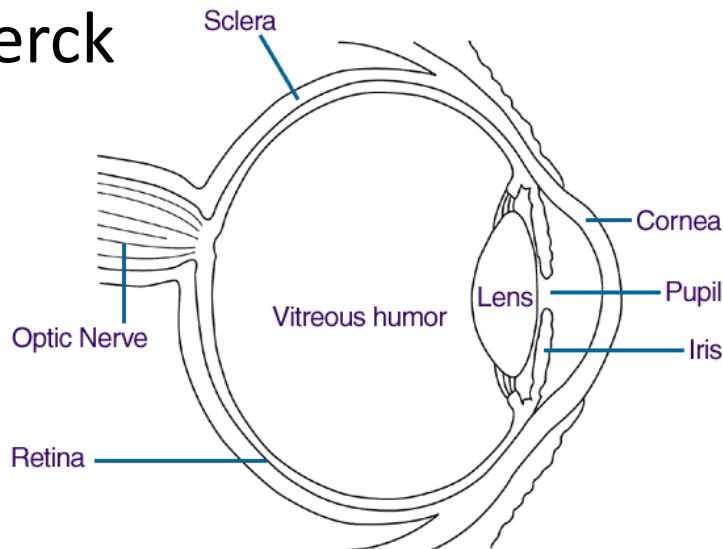
Collaboration Grant with Large Pharmaceutical Company (2019-20)

- 2-year *funded* collaborative project with a large pharmaceutical company on the enhancement & validation of GastroPlus mechanistic pulmonary models:
 - Handle volatile materials/vapors
 - Improved deposition predictions through ion trapping effects



Cooperation Grant with the FDA (2014-20)

- 6-year *funded* collaborative project with the FDA Office of Generic Drugs on the further development & validation of GastroPlus mechanistic models for ocular delivery
- Consortium members: FDA, Alcon, Santen, GSK, Senju, Merck



Research Collaboration Agreement with the FDA (2014-19)

- 5-year collaborative project with the FDA Office of Testing and Research on the utility of GastroPlus Mechanistic Absorption Modeling (MAM) and IVIVCs to predict complex absorption characteristics
 - Goal is to facilitate drug product development by decreasing regulatory burden through modeling & simulation

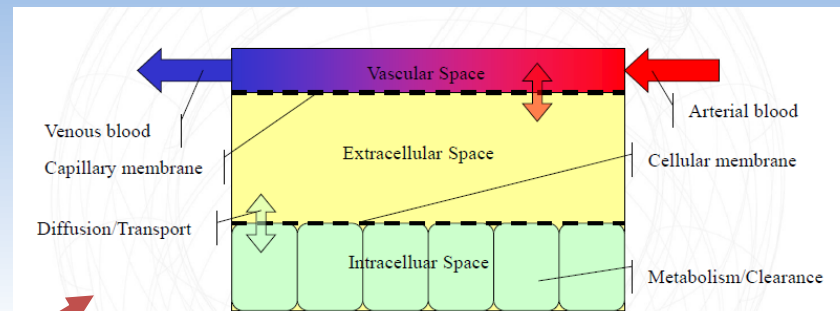
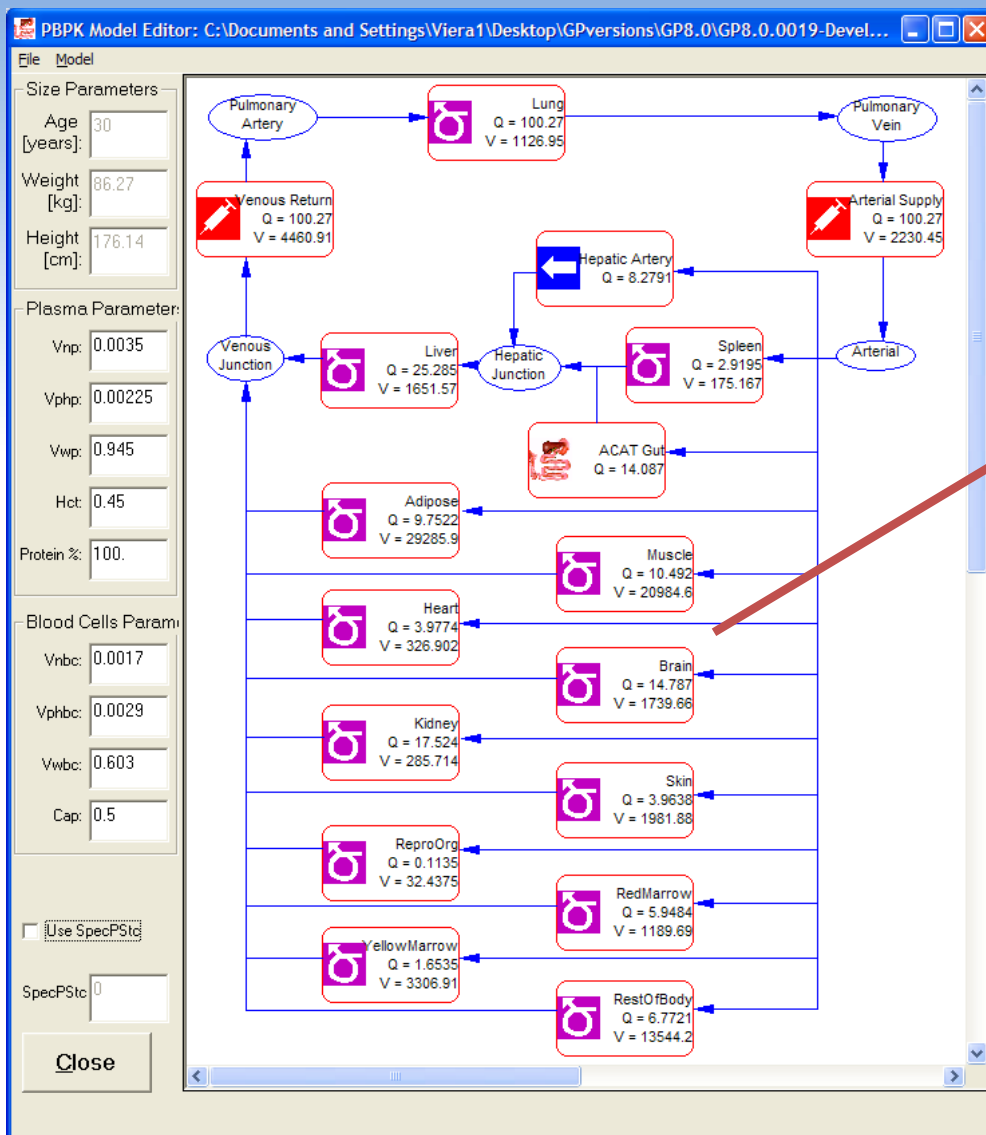
The Virtual BE Trial Simulator™ Project

- New funded collaboration with large pharma sponsor:
 - Automation of multiple virtual BE trial simulations w/specific trial designs
 - Integration of intrasubject variability methods
 - Improved statistical analyses and reporting options
 - Implementation of CMC and physiological covariate models
 - Incorporation of audit trails for the virtual BE trial simulation activities
 - Population parameter fitting to link pharmacometrics and PBPK modeling approaches
- First version likely available in summer 2020

Improvements to the ACAT™ Model

- New funded collaboration with large pharma sponsor:
 - Literature review to identify mechanisms, develop and parameterize models to improve predictions of drug concentrations in gut tissue
 - Add option to modify gut perfusion to account for increased liver blood flow under fed conditions
 - Mechanistically model luminal conversion processes
 - Permit the use of observed gut lumen, enterocyte, and whole gut tissue concentrations as target profiles for optimization of model parameters in GastroPlus.
 - Characterize mechanisms leading to drug distribution between the enterocyte layer, gut vascular space and gut tissue
- First version likely available in summer 2020

What's Defined in a PBPK Model?



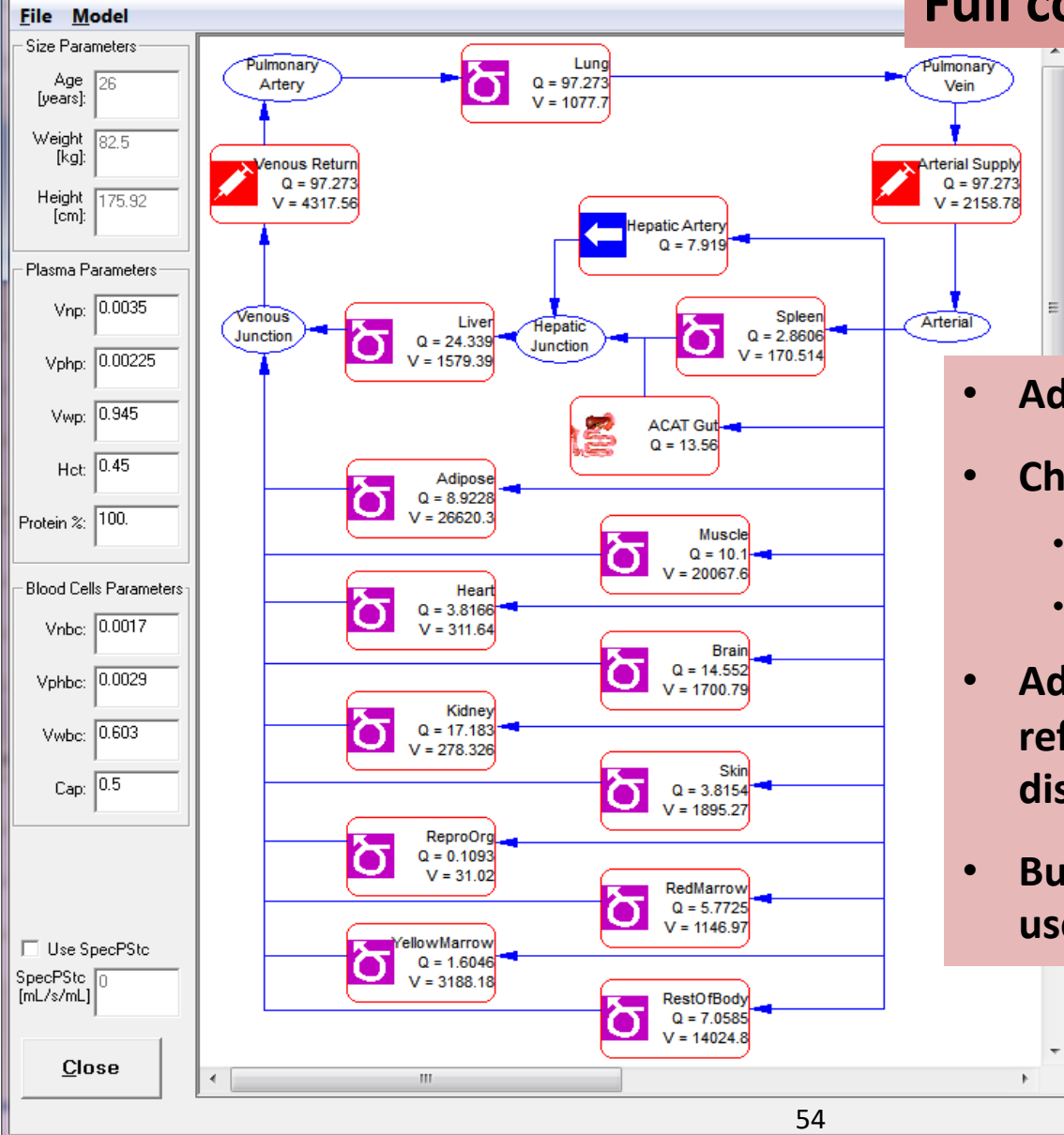
$$V_t \frac{dC_t}{dt} = \left(Q \times C_{bi} - \frac{Q \times C_t \times R_{bp}}{K_p} - CL_{int,u} \left(\frac{C_t \times f_{u,p}}{K_p} \right) \right)$$

- Each compartment represents a tissue:
 - Specific volume(s) *
 - Blood perfusion rate *
 - Enzyme/transporter expression levels *
 - Volume fractions of lipids & proteins *
 - Tissue:plasma partition coefficient (K_p)
 - Estimated from drug properties:
 - logD vs. pH
 - pKa(s)
 - Plasma protein binding
 - Blood:plasma concentration ratio

PBPKPlus Module

PBPK Model Editor: C:\C Drive Content\GastroPlus Training Slides\Midazolam PBPK -7.1AP_GF...

Full control over the physiology



- Add or remove tissues
- Change tissue type
 - Perfusion-limited tissue
 - Permeability-limited tissue
- Adjust tissue parameters to reflect different physiology, disease state, ...
- But default settings are used most often

PBPK Modeling of Biologics

Drug Specific Parameters

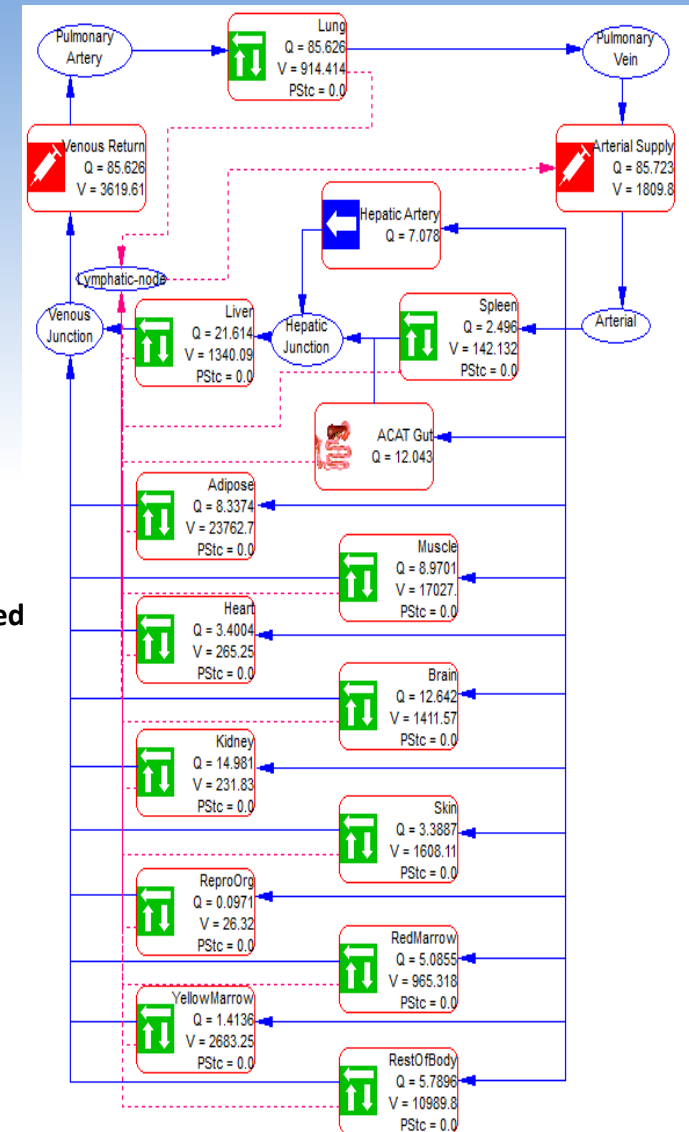
Vascular reflection coefficient
 Lymphatic reflection coefficient
 Vascular Rate Fraction
 Endosomal Uptake Rate
 Recycle Rate
Kon, FcRn
Koff, FcRn
Kdeg
Antigen Kon
Antigen Koff
Antigen Kint
 (bold indicates parameters that may be optimized based on available data)

PBPK

Physiological Parameters

Organ size
 Tissue composition
 Blood perfusion rate
 Lymph flow rate
 FcRn concentration

Age
 Species
 Gender
 Weight



Application Areas at the FDA Office of Generic Drugs (2008-2016)

| | Potential Applications | Current Status |
|---|--|---|
| Dissolution Method and Acceptance Criteria | <i>Justify/support bio-predictive dissolution method</i> | <ul style="list-style-type: none"> • <i>Use the verified PBPK/absorption model combined with bioequivalence clinical study and dissolution profiles generated to show that the proposed dissolution method can reject non-BE (bioequivalence) batch</i> |
| | <i>Set clinically relevant dissolution acceptance criteria</i> | <ul style="list-style-type: none"> • <i>Allow dissolution acceptance criteria to go beyond target $\pm 10\%$ range</i> • <i>Additional evidence (data) needed to validate model and confirm predictive performance</i> |
| Set clinically relevant drug product specifications for CMAs and CPPs | <i>CMAs (particle size, polymorphic form)</i> | <ul style="list-style-type: none"> • <i>Predict particle size distribution (PSD) limits which would result in similar in vivo performance to the target (clinical batch)</i> • <i>Predict the effect of polymorphic form on in vivo performance of drug product</i> |
| | <i>CPPs (milling method, pressure force/hardness)</i> | <ul style="list-style-type: none"> • <i>Predict the effect of milling method on the bioequivalence of drug product (e.g. pre- and post-change of milling method)</i> • <i>Used to justify specification range of compression force based on the predicted in vivo performance</i> |
| Risk assessment | <i>Evaluation of the risk</i> | <ul style="list-style-type: none"> • <i>Quantitative assessment</i> |